

DIATERMO MB 300 T-400 T

ELECTROSURGICAL UNIT

USER MANUAL



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IMPORTANT

This instruction manual represents an essential part of the HF electrosurgery unit and must be kept available to the operating staff at all times. It is of paramount importance to carefully read and fully understand all instructions and guidelines before attempting any use of an active electrode.

It is imperative to diligently follow all warnings and safety instructions. Please ensure that this documentation is included with the device in case it is transferred to another team.

In the event of technical assistance being required, please contact LED SpA.

Produttore / Manufacturer

LED SpA

PROGETTAZIONI E PRODUZIONI ELETTRONICHE

Via M.T.Cicerone 138 03100 FROSINONE (FR) ITALIA

www.led.it

INTRODUCTION

STANDARD AND OPTIONAL COMPOSITION

Description		DIATERMO	
		MB 300 T	MB 400 T
Electrosurgical unit code		GMA10400.T50	GMA10400.T60

DIATERMO MB		300 T	400 T
Code	Description	Quantity	
00100.01	Power supply cable 5m SIE-IEC	■/1	■/1
00205.00	PENCILS S – Handpiece with switch	■/1	■/1
00305.06_S	Double water-proof footswitch	■/2	■/2
00306.06	Double water-proof footswitch with selector	■/1	■/1
00401.20	NEUTRAL - Steel Neutral Split Electrode FLEX S 120x210mm	■/1	■/1
00404.08_S	CONNECTION - Cable for neutral electrode disposable type 5365/6429/FLEX	■/1	■/1
152-110	ELECTRODE - Blade electrode 7 cm	■/3	■/3
152-115	ELECTRODE - Blade electrode 16 cm	■/3	■/3
152-150	ELECTRODE - Ball electrode ø 4mm 6 cm	■/3	■/3
00100.00	Power supply cable 2m IT-IEC	○	○
00100.03	Power supply cable 2m SIE-IEC	○	○
00100.04	Power supply cable 2m USA-IEC	○	○
00100.05	Power supply cable 2m GB-IEC	○	○
00100.07	Power supply cable 2m BR-IEC	○	○
00100.09	Power supply cable 2m AU-IEC	○	○
00100.10	Power supply cable 5m JP-IEC	○	○
00205.40	PENCILS S – Handle with switch (for electrode 4mm)	○	○
00206.00	PENCIL - Handle without switch	○	○
00206.40	PENCIL - Handle without switch (for electrode 4mm)	○	○
00306.06	Double water-proof foot switch TOUCH HP with selector	○	○
00401.01	NEUTRAL - Steel Neutral Electrode 24x16 cm with cable	○	○
00401.03	NEUTRAL - Steel Neutral Electrode 24x16 cm with cable autoclavable	○	○
00401.10	NEUTRAL - Steel Neutral Electrode FLEX 120x210mm	○	○
00401.11	NEUTRAL - Steel Neutral Electrode FLEX 120x210mm with cable	○	○
00401.12	NEUTRAL - Steel Neutral Electrode FLEX 120x210mm with cable autoclavable	○	○
00401.21	NEUTRAL - Steel Neutral Split Electrode FLEX S 120x210mm with cable	○	○
00401.22	NEUTRAL - Steel Neutral Split Electrode FLEX S 120x210mm with cable autoclavable	○	○
00402.00	CONNECTION - Monopolar cable M4-F4 3mt	○	○
00402.01	CONNECTION - Monopolar cable M4-F2.8 3mt	○	○
00402.02	CONNECTION - Monopolar cable M4-MP4 3mt	○	○
00402.03	CONNECTION - Monopolar cable M4-EU 3mt	○	○
00402.04	CONNECTION - Monopolar cable M4-F2.M 3mt	○	○
00404.07	Cable for connection neutral electrode F7915/F7930	○	○
00404.09	CONNECTION - Cable for neutral electrode disposable type 5365/6429/FLEX autocl.	○	○
00411.00	CONNECTION - Bipolar cable EUR	○	○
00413.00	CONNECTION - Bipolar cable 3mt Artery Sealer EUR	○	○
00414.00	CONNECTION - Bipolar cable 3mt US	○	○
00415.00	CONNECTION - Bipolar cable 3mt ENDO1 (F4-F2)	○	○
00416.00	CONNECTION - Bipolar cable 3mt ENDO2 (MP2-F2)	○	○
00417.00	CONNECTION - Bipolar cable 3mt ENDO3 (MP2-F4)	○	○

DIATERMO MB		300 T	400 T
Code	Description	Quantity	
00418.00	CONNECTION - Bipolar cable 3mt SCISS (F2.4-F2.4)	○	○
00420.00	Reusable handle with finger switch for Argon	○	○
00420.12	Argon coagulation electrode 150mm	○	○
00420.10	Argon coagulation electrode 75mm	○	○
00420.14	Argon coagulation electrode 370mm	○	○
00430.00	Connection cable for flexible Argon probes, 2.5mt	○	○
00430.10	Monopolar flexible Argon probe 1.5mm, 1.5mt	○	○
00430.12	Monopolar flexible Argon probe 1.5mm, 3mt	○	○
00430.20	Monopolar flexible Argon probe 2.3mm, 1mt	○	○
00430.22	Monopolar flexible Argon probe 2.3mm, 2.2mt	○	○
00430.24	Monopolar flexible Argon probe 2.3mm, 3mt	○	○
00430.30	Monopolar flexible Argon probe 3.2mm, 2.2mt	○	○
0350	Disposable Neutral electrode (F7805)	○	○
10500.30	SURTRON ABC Pressure reducer UNI11144 Gruppo VIII	○	○
110-750NS	BIPOLAR - Bipolar Artery Sealer 27cm TIP 3mm	○	○
110-755NS	BIPOLAR - Bipolar Artery Sealer 25,5cm TIP 3mm	○	○
110-760NS	BIPOLAR - Bipolar Artery Sealer 17cm TIP 2mm	○	○
152-112	ELECTRODE - Blade curved electrode 7 cm	○	○
152-122	ELECTRODE - Needle curved electrode 7 cm	○	○
152-125	ELECTRODE - Needle electrode 13 cm	○	○
152-130	ELECTRODE - Ball electrode ø 2mm 6 cm	○	○
152-132	ELECTRODE - Ball curved electrode ø 2mm 6 cm	○	○
152-140	ELECTRODE - Ball electrode ø 3mm 6 cm	○	○
152-142	ELECTRODE - Ball curved electrode ø 3mm 5 cm	○	○
152-145	ELECTRODE - Ball electrode ø 3mm 14 cm	○	○
152-152	ELECTRODE - Ball curved electrode ø 4mm 6 cm	○	○
152-160	ELECTRODE - Ball electrode ø 5mm 6 cm	○	○
152-162	ELECTRODE - Ball curved electrode ø 5mm 6 cm	○	○
152-165	ELECTRODE - Ball electrode ø 5mm 14 cm	○	○
152-175-10	ELECTRODE - Loop electrode 10x10 l.15 cm	○	○
152-190-13	ELECTRODE - Loop electrode 20x13 l.15 cm	○	○
152-190-20	ELECTRODE - Loop electrode 20x20 l.15 cm	○	○
152-195	ELECTRODE - Conization electrode 13 cm	○	○
310-110-05	BIPOLAR - Bipolar Forceps 11,5cm TIP0.5mm	○	○
310-112-05	BIPOLAR - Bipolar Forceps Curved 11,5cm TIP0.5mm	○	○
310-140-10	BIPOLAR - Bipolar Forceps 20cm TIP 1mm	○	○
310-140-20	BIPOLAR - Bipolar Forceps 20cm TIP 2mm	○	○
310-142-10	BIPOLAR - Bipolar Forceps Curved 20cm TIP 1mm	○	○
310-142-20	BIPOLAR - Bipolar Forceps Curved 20cm TIP 2mm	○	○
310-180-10	BIPOLAR - Bipolar Forceps Angled 20cm TIP 1mm	○	○
310-180-20	BIPOLAR - Bipolar Forceps Angled 20cm TIP 2mm	○	○
310-182-10	BIPOLAR - Bipolar Forceps Angled Curved 20cm TIP 1mm	○	○
310-185-10	BIPOLAR - Bipolar Forceps Angled Curved 20cm TIP 1mm	○	○
310-510	BIPOLAR - Bipolar electrode 20cm – direct	○	○
310-550	BIPOLAR - Bipolar electrode 20cm – curved 1	○	○
310-590	BIPOLAR - Bipolar electrode 20cm – curved 2	○	○
330-134-20	MONOPOLAR - Monopolar Forceps 20cm TIP2mm	○	○
330-160	MONOPOLAR - Monopolar Surgical Scissors 18cm	○	○
410-100-15	BIPOLAR – Bipolar Forceps Clamp Scissors 15cm	○	○
410-100-19	BIPOLAR – Bipolar Forceps Clamp Scissors 19cm	○	○
410-200-18	BIPOLAR – Bipolar Forceps Scissors 18cm	○	○
410-200-21	BIPOLAR – Bipolar Forceps Scissors 21cm	○	○
410-200-23	BIPOLAR – Bipolar Forceps Scissors 23cm	○	○
6429A	NEUTRAL - Steel Neutral Electrode 24x16 cm	○	○
F7915	Conductive rubber neutral electrode without cable	○	○

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F7930	Conductive rubber split neutral electrode without cable	○	○
TRST001	Trolley for SURTRON TOUCH HP	○	○
TRCYLSUP01	Support for Cylinder	○	○

■/ Pcs = STANDARD

○= OPTIONAL

GENERAL DESCRIPTION

The high-frequency electrosurgical equipment is capable of providing current for monopolar cutting, coagulated cutting with different levels of coagulation, in both monopolar and bipolar modes. In bipolar coagulation mode, it is possible to activate a tissue impedance detection system with automatic start and automatic stop once coagulation is reached (AUTOSTART - AUTOSTOP functions). In addition, a specific function can be used to perform vascular and venous synthesis and coagulation by means of radiofrequency vessel sealing.

A total of ten different operating modes and power levels can be memorised and recalled for easy use.

You have the option of using single-plate neutral reference electrodes or electrodes with a split conductive zone to monitor the patient's impedance stability during surgery.

Control of the unit is via the display. The power input is located on the rear panel. The units are equipped with automatic control systems that monitor internal parameters and report any damage or errors. The operating parameters used are constantly stored, so that the last parameters selected are recalled each time the unit is switched on or the operating method is changed.

The sound volume adjustment can be customised, allowing each operator to choose the level best suited to the working environment.

The units can be controlled via handpieces with or without pushbuttons, including a dual foot control. A bipolar clamp can be connected to the unit for bipolar functions.

INTENDED USE

Medical device intended for temporary use for surgical operations in which cutting and/or coagulation of soft tissues is required, with a monopolar and/or bipolar technique, for survey minor and/or major in open and/or intra-operative percutaneous and/or endoscopic and/or laparoscopic.

The **DIATERMO MB 300 T** and **DIATERMO MB 400 T** equipment are designed for being used in the following sectors:

Description	DIATERMO MB 300 T	DIATERMO MB 400 T
Electrosurgical unit code	GMA10100.T50	GMA10100.T60
Endoscopy	•	•
Gastroenterology	•	•
General Surgery	•	•
Gynaecology	•	•
Neurosurgery	•	•
Orthopaedics	•	•
Otorhinolaryngology	•	•
Paediatric Surgery	•	•
Plastic Surgery	•	•
Pneumology	•	•
Thorax Surgery	•	•
Trans Urethral Resection (TUR)	•	•
Urology	•	•
Vascular Surgery	•	•

• = Usable

INTENDED USER

Device for professional use. Use of the equipment is restricted to medical personnel with medical degrees specializing in high frequency electrosurgery.

INTENDED PATIENT POPULATION

Adults - Men and women (≥18 years), excluding patients in the contraindications section.

ELECTROPHYSICAL PRINCIPLES

In electrosurgical interventions the traditional use of surgical blade is substituted by an electrosurgical needle that allows for fast and effective cut and coagulation of the targeted tissue.

The electrosurgical needle operates on the principle of converting electrical energy into heat and consists of the following components:

- A radiofrequency sinusoidal oscillator (0.4 - 4MHz).
- A wave packet generator with a packet repetition frequency of 15 – 30 kHz.
- A mixer for transferring the waveform to the power amplification block, either for cutting, coagulation, or a signal obtained from an appropriate combination of the two.
- A power amplifier block capable of supplying the required power in terms of current and transmitting the amplified signal to the electrodes through a transformer.
- A safety circuit for the return electrode, designed to detect any cable interruptions and deactivate the radiofrequency delivery.
- A specially shaped active electrode (handpiece).
- A return electrode (neutral) that completes the circuit through the patient.

Electric current flowing through biological tissue usually can cause:

1. ***Joule Effect***
2. ***Faradic Effect***
3. ***Electrolytic Effect***

1. ***Joule Effect***

In biological tissue, when passed through by the electric current delivered by the electrosurgical scalpel, heating (Joule effect) is produced, which is dependent on tissue-specific electrical resistance, current density, and application time and can result in various cellular transformations.

$$Q = I^2 \times R \times T$$

The influence of the thermal effect (Joule effect) is realized by:

- **Current Intensity and output power**
- **Modulation level**
Parameters that can be interpreted from the waveform of the high-frequency current produced by the generator.
- **Electrode shape**
Pointed or rounded as required, it is very small in size; therefore, the current density on the tip surface [$A \cdot m^{-2}$] is very high. Thin-section electrodes create a high current density, and high temperature, promoting cutting action. Those with a large surface area create a lower current density, and lower temperature, realizing a coagulation effect.

- **State of active electrode**

Thermal effects can be related to the resistance of the human body to which the contact resistance of the electrode must be added. It is essential to keep the active electrodes perfectly clean in order not to have a reduction in the effects.

- **Characteristics of the tissue**

The resistive characteristics change according to the biological tissues.

Biological Tissue (range from 0,3 to 1 MHz)	Metals
Blood $0,16 \times 10^3 \Omega$	Silver $0,16 \times 10^{-5} \Omega$
Muscle, kidney, heart $0,2 \times 10^3 \Omega$	Branch $0,17 \times 10^{-5} \Omega$
Liver, spleen $0,3 \times 10^3 \Omega$	Gold $0,22 \times 10^{-5} \Omega$
Brain $0,7 \times 10^3 \Omega$	Aluminium $0,29 \times 10^{-5} \Omega$
Lung $1,0 \times 10^3 \Omega$	
Fat $3,3 \times 10^3 \Omega$	

(Example of specific resistances of organic and metallic materials)

Based on the temperature achieved and according to the pulse forms used, different techniques of using radiofrequency current on the human body are recognized as follows:

- **Coagulation**

Temperatures of 60 to 70 °C in the area around the active electrode cause slow heating of the intracellular fluid, the water contained in the cell evaporates, and a clotting action is achieved that stops bleeding.

- **Cut**

Temperatures above 100 °C in the area surrounding the active electrode result in the vaporization of the intracellular fluid and explosion of the cell. The vapor present around the electrode triggers an intercellular chain reaction in the direction in which the active electrode is handled, also transmitting the vaporization energy to the immediately surrounding tissues.

Electrotomy is, therefore, not mechanical resection. If the temperature reaches 500 °C, tissue carbonization occurs with a cauterizing action.

- **Mixed currents**

These are obtained by combining the effects of coagulation and electrotomy. A reduction in bleeding occurs during a cutting procedure, or as a cut that develops a substantial layer of eschar. The high frequencies used by the electrosurgical scalpel, however, do not allow the electromagnetic field to penetrate matter and cause the current to flow through the conductor more on the outermost surface, decreasing exponentially and becoming negligible in the center of the conductor's cross-section. This effect, called the 'skin effect,' results in a decrease in the useful cross-sectional area for the passage of a current, and an increase in the electrical resistance of the material, and becomes a major problem in the neutral electrode. In fact, in this electrode the current density is very high (KA/m^2) at the edge, where excessive temperature rise due to the 'Joule effect' causes burns to the patient. Therefore, it is no accident that burns to the patient, which has occurred

in surgical procedures, have the shape of the edge of the neutral electrode. To reduce the risk of burns, it is necessary to dose the delivered power ($I^2 \cdot t$) appropriately and follow the rules for applying the neutral electrode to the patient (see SAFETY chapter).

2. Faradic Effect

Pulsed electric current causes neuro-muscular stimulation, originating from the stimulation of the physiological process of ion exchange, which is responsible for the transmission of stimuli that cause muscle spasms and cardiac phenomena of extrasystole and ventricular fibrillation.

The effect of these stimuli is known as the faradic effect and is expressed by:

$$R = I / \sqrt{F}$$

The physiological system of stimulus transmission follows a limiting curve in which pulsed or low-frequency currents generate a pacing pulse. With the high-frequency alternating current (above 200 kHz), which is used in electrosurgery, there are no neuromuscular reactions (the change of polarity is so fast that it does not affect the patient at the level of neuro-muscular reactions), let alone electrolyte damage to the body.

For this reason, all high-frequency generating equipment for surgical use (electrosurgery) works on base frequencies above 300 kHz so as not to introduce electrical stimulation.

3. Electrolytic Effect

The use of high-frequency currents reduces the electrolytic effect (ionic separation) in tissues due to the very short unidirectional conduction period of the current.

OPERATIVE TECHNICS

MONOPOLAR CUT

Monopolar cutting is a technique used to dissect biological tissue by directing a high-frequency, high-density electrical current from the active electrode's tip. This current generates intense molecular heat within the cells, causing them to rupture. As the electrode moves through the tissue, it shears and destroys cells sequentially. This movement prevents the lateral spread of heat within the tissue, confining the destruction to a single line of cells.

For precise cutting with minimal thermal impact and limited hemostasis, a pure sine wave current without modulation is preferred. This allows for precise control and safe use without harming adjacent bone. However, some level of modulation in the current is desirable to facilitate effective coagulation during the cutting process, making electrosurgery an advantageous technique.

The following rules help the operator achieve a good cut:

- Keep the tissue moist but not wet.
- Maintain the electrode perpendicular to the tissue.
- Activate the output circuit before making contact with the tissue.
- Keep the electrode tip clean (for this purpose, you can use optional electrode-cleaning sponges with code F7520).
- Allow the tissue to cool before making a new cut.

When the output power level is adequate, you can expect to achieve:

- No resistance when moving the electrode through the tissue.
- No change in the color of the cut surfaces.
- No residual tissue fibers on the electrode.

MONOPOLAR COAGULATION

When an increase in temperature occurs, caused by the heat generated through the Joule effect in the tissue, thermal coagulation takes place. This process involves the partial solidification of organic liquids and the precipitation of colloidal substances. Specifically, within the blood, fibrin forms, which, as it solidifies, can obstruct blood vessels.

To achieve coagulation using an electrosurgical scalpel, it's essential to provide the active electrode with an intermittent current. This prevents excessive heat generation, which could lead to cell explosion and tissue cutting, allowing for controlled heating instead. This controlled heating causes the water within the cells to escape without destroying them. However, even with intermittent current, if the current intensity is too high, it can still result in a cutting effect.

Active electrodes well-suited for coagulation purposes include those with ball, plate, or lance shapes, used laterally.

Coagulation can be achieved through different methods:

- **Coagulation by Desiccation**

This is achieved by supplying the electrode with low voltages to prevent the generation of sparks (ensuring that the action obtained is pure coagulation without any cutting effect). The electrode is placed in direct contact with the tissue, and the amount of heat generated on contact dries it out. Typically, coagulated cellular surfaces act as an insulating layer, preventing heat from subsequent current applications from penetrating too deeply. The current normally used for coagulation is modulated. Depending on the modulation percentage, you get a balance between precision in cutting, effectiveness in hemostasis, and tissue destruction. Greater modulation of the current leads to a more jagged cut, greater depth of tissue destruction, but more effective coagulation.

The following rules help the operator achieve good coagulation:

- Select a ball electrode or a thick wire electrode.
- Locate the bleeding vessel after excess blood has been dried from the area.
- Gently touch the bleeding vessel before activating the electrode.
- Cease electrode activation as soon as the tissue whitens to avoid damaging it.
- Keep the electrode tip clean (you can use optional electrode-cleaning sponges with code F7520).

- **Coagulation by Fulguration or Spray**

This technique involves supplying the electrode with high voltages, creating one or more electrical arcs that extend over the tissue without direct contact. These arcs extinguish and reappear in different locations. The resulting heat is distributed across a larger tissue surface compared to the single arc used for cutting, emphasizing coagulation.

This method is particularly effective for treating extensive surfaces with diffuse and superficial bleeding, such as in hepatic resection. It is also suitable for achieving coagulation in open sternum cardiac surgeries. The distributed heat and controlled electrical arcs make this method ideal for minimizing blood loss and promoting effective coagulation on sizable tissue areas.

- **Coagulation with Anatomical Forceps by Clamping**

The most commonly used coagulation technique involves blocking the blood flow by applying clamping pressure at the end of the forceps. After clamping the tissue portion or the blood vessel where coagulation is needed, the active electrode is brought into contact with the proximal metal part of the forceps. The high-frequency activation must occur after this contact (forceps - active electrode) to avoid the Faradic effect (initiation of an electrical discharge that uses air as a conductor), which could cause electrical shock, burns to the operator, etc.

BIPOLAR CUT AND COAGULATION

In contrast to monopolar techniques, the bipolar technique involves a very localized passage of high-frequency current through a small portion of tissue. Bipolar forceps, with varying dimensions and shapes, are utilized in this technique. These forceps have active and neutral electrodes at their distal ends. By clamping the targeted tissue between the forceps' ends, the high-frequency current passes from one end to the other, treating the tissue as an electrical bridge.

Bipolar Cut:

The bipolar cut entails dissecting biological tissue through the passage of high-density current concentrated between the two points of the bipolar forceps. This method is gaining significant interest, especially for its enhanced safety and its compatibility with endoscopic and non-invasive surgical techniques.

Bipolar Coagulation:

Bipolar coagulation involves the haemostasis of small blood vessels within the body tissue between the two points of the forceps. When the current density is reduced, the resultant effect is surface desiccation of the cells without deep penetration, leading to coagulation.

The bipolar technique is considered highly safe because the direction of the high-frequency current is always predetermined, eliminating unknown factors and potential errors. Moreover, the power levels used in bipolar techniques are lower than those employed in monopolar techniques. Due to these safety factors, the bipolar technique is often preferred in critical surgical operations. However, it is crucial to keep the distal ends of the forceps clean during the operation to prevent the accumulation of coagulated tissue, which could impede current passage and promote tissue adhesion.

While the application of a neutral electrode (compulsory in monopolar techniques) is not necessary in the bipolar technique, it is advisable for practical reasons, especially during the initial preparatory phase of the operation.

CONTRAINDICATIONS

The use of electrosurgery is contraindicated in patients:

- pacemaker carriers
- with stimulation electrodes
- with metallic prostheses
- with serious blood pressure imbalances
- with serious diseases of the nervous system
- with serious kidney failure
- in state of pregnancy.

In the context of electrical surgery, burns due to high frequency are the main causes of burns caused to the patient, but they are not the only ones involved. One can also get necroses by compression, allergic reactions to disinfectants, gas sparks or flammable liquids.

Some of the causes of burns are to be attributed to:

- insufficient medical equip training about all modalities to avoid or reduce the risks of burns by using HF electrosurgical units
- use of disinfectants with high alcohol content
- incorrect position of the patient during the electrosurgical operation
- contact between active electrode and the skin
- contact with liquid
- long application of HF currents
- incorrect application of the patient-plate.

To avoid or reduce the risks associated with the use of high frequency electrosurgery, it is necessary to respect the rules and safety measures illustrated in the following chapter.

SAFETY

WARNING: Electrosurgery carries inherent risks, and improper usage of any component within the electrosurgical system can result in severe burns to the patient. It is absolutely crucial that you meticulously read and comprehensively understand all instructions before attempting to utilize an active electrode. Neither the manufacturer nor any retailers can be held liable for any harm or damage, whether direct or indirect, caused to individuals or equipment due to the incorrect use of the device and its accompanying accessories.

The accessories provided with this unit are designed to be compatible specifically with this unit and may not work with other electrosurgical units. Prior to connecting any additional accessories to this unit, the user must confirm that these accessories possess insulation characteristics that align with those of this unit (please refer to the "TECHNICAL CHARACTERISTICS" section for details). It is strongly allowed to assess the packaging integrity of sterile accessories before their initial use.

ATTENTION

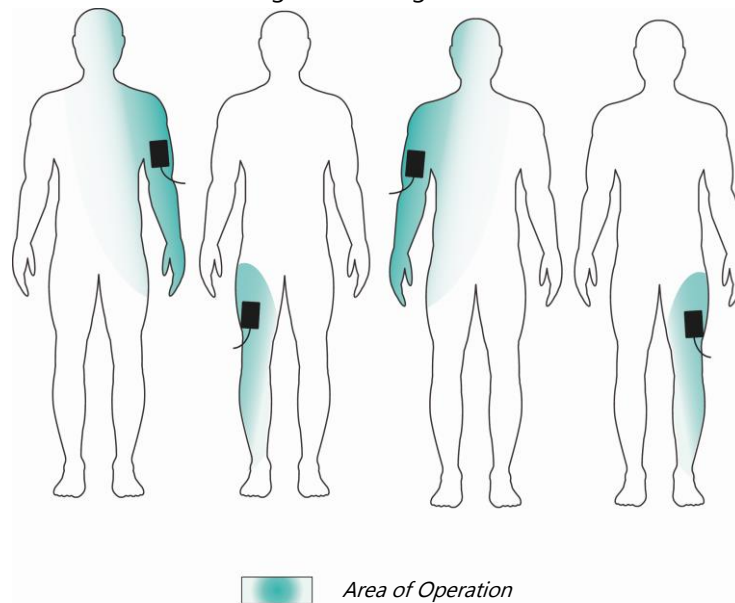
- DO NOT USE on patients with electronic implants such as cardiac pacemakers without consulting a qualified professional (e.g., a cardiologist). There is a potential risk of interference with the functioning of the electronic implant or damage to the implant itself.
- DO NOT USE in the presence of flammable anaesthetics or oxidizing gases (such as nitrous oxide (N₂O) and oxygen) or near volatile solvents (such as ether or alcohol) as explosions may occur.
- DO NOT PLACE instruments near or in contact with flammable materials (such as gauze or surgical drapes). Activated or heated instruments can cause fires.
- When not in use, store instruments in a clean, dry, and highly visible area away from direct patient contact. Inadvertent contact with the patient can result in burns.
- INSPECT instruments and cables for damage before each use, especially the insulation of laparoscopic/endoscopic instruments. This inspection can be carried out visually under magnification or with a high-voltage insulation testing device. Insulation failures can lead to burns or other injuries to the patient or the operator.
- The surface of the active electrode may remain sufficiently hot to cause burns even after RF current is deactivated.
- Due to concerns about the potential carcinogenic and infectious properties of electrocautery byproducts (such as tissue smoke plumes and aerosols), protective eyewear, filtration masks, and effective smoke evacuation equipment should be used in both open and laparoscopic procedures.
- Only connect adapters and accessories to the electrosurgical unit when the power is OFF. Failure to do so may result in patient or operating room personnel injury or electric shocks.
- If the device is powered with argon, warnings regarding gas embolisms must be included.
- If the instrument is reusable, a warning should be included that visual inspection alone may not be sufficient to ensure intact insulation.
- DO NOT ACTIVATE the instrument when it is not in contact with the target tissue, as this could cause injuries due to capacitive coupling with other surgical equipment.

- ASPIRATE fluids from the area before activating the instrument. Conductive fluids (e.g., blood or saline) in direct contact with or in proximity to an active electrode can carry electrical current or heat away from the target tissues, potentially causing unintended patient burns.
- DO NOT USE with hybrid systems, i.e., a combination of metal and plastic, when using monopolar active components. This can result in burns at alternative sites due to capacitive coupling. Use only all-metal or all-plastic systems.
- Before increasing the intensity, verify the adhesion of the neutral electrode and its connections. Apparent low power or device malfunction at normal operating settings may indicate improper neutral electrode application or poor contact in its connections.
- This unit has a CQM system; please note that the loss of secure contact between the neutral electrode and the patient will not trigger an alarm unless a compatible monitoring neutral electrode (split neutral electrode) is used.
- CAUTION: Set the intensity to the lowest level necessary to achieve the desired effect.
- CAUTION: Keep the active electrodes clean. Accumulated eschar may reduce the tool's effectiveness. Do not activate the instrument during cleaning. Operating room personnel may be injured.
- Any serious incidents related to the device must be reported to LED SpA (via Selciatella n.40, 04011 Aprilia (LT) ITALY) and the competent authority:
Ministero della salute – Direzione generale dei dispositivi medici e del servizio farmaceutico
Viale Giorgio Ribotta, 5 – Roma
E-mail: segr.dgfdm@sanita.it
Tel.: +39 06 5994 3199 / +39 06 5994 3207

PRECAUTIONS

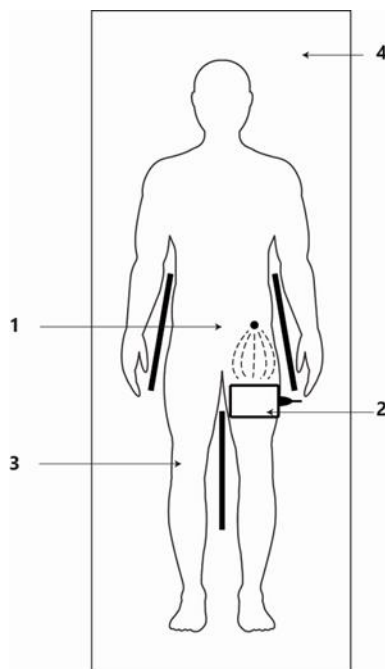
The following precautions are crucial for minimizing the risk of inadvertent burns:

- Ensure the secure and complete attachment of the neutral electrode to the patient's body, preferably at the extremities and as close to the surgical site as possible. Avoid connecting the neutral electrode to bony protrusions, prosthetic devices, areas with scar tissue, regions susceptible to fluid accumulation, or areas with a thick layer of subcutaneous fat. The application site should be free from hair, dry, and clean. Avoid using alcohol for skin cleaning. Except for veterinary medicine applications, refrain from using electrode gel.



- When using single-use neutral electrodes, always adhere to the provided expiry dates.
- For multi-use electrodes, ensure that the fixation systems in place guarantee stability during use.
- When applying the neutral electrode, avoid a transverse path and instead favour a vertical or diagonal path, especially when using a bipartite neutral electrode. This helps distribute current evenly across the surface of the neutral electrode and reduces the risk of patient burns.
- If you encounter difficulty in correctly applying the neutral electrode, consider using the bipolar technique instead of the monopolar approach, if feasible.
- To prevent the patient from coming into contact with earthed metallic parts or components with significant grounding capacity (such as an operating table or supports), it is allowed to use an antistatic drape for this purpose.

- To avoid skin-to-skin contact (e.g., between the arm and trunk, between the legs, or on the breasts), it's allowed to insert dry gauze. Additionally, ensure that body areas prone to profuse sweating are kept dry.



1. Active Electrode – 2. Neutral Electrode
3. Dry Gauze – 4. Antistatic Drape

- When using both an electrosurgical scalpel and a physiological monitoring device on the same patient, you must place all monitoring electrodes as far away from the surgical electrodes as possible. Needle monitoring electrodes are discouraged. In any case, it is allowed to use monitoring systems that incorporate high-frequency current-limiting devices.
- Position surgical electrode cables in a manner that prevents contact with the patient or other conductive materials. Active electrodes that are not in use should be isolated from the patient.
- Consider utilizing bipolar techniques when operating on body parts with a relatively small cross-sectional area. This helps prevent unintended coagulation.
- Set the output power level to the lowest effective setting for the intended purpose, minimizing the risk of excessive tissue damage.
- If the electrosurgical unit exhibits an obvious low output level or operates incorrectly, even when set up for normal power delivery, this could indicate issues with the application of the neutral electrode or poor contact in the neutral electrode connections. Therefore, it is essential to verify the proper placement and connections of the neutral electrode before considering higher power settings.
- Avoid the use of flammable anesthetics or oxidizing gases, such as nitrous oxide (N₂O) and oxygen, especially in chest or head operations, unless they can be safely aspirated. Whenever possible, opt for non-flammable substances for cleaning and disinfection purposes. If flammable substances are used for cleaning, disinfection, or as solvents for adhesives, they should be allowed to completely evaporate before using the electrosurgical unit. There is a risk of flammable solutions accumulating under the patient or in cavities like the umbilicus and vagina. Any fluid in these areas should be

removed before using the device. It's important to consider the presence of endogenous gases as well.

- Be aware that certain materials, such as cotton wool or gauze impregnated with oxygen, may ignite due to sparks produced by the appliance under normal conditions. Take necessary precautions to prevent such incidents.
- Patients with pacemakers or pacing electrodes are at risk of interference with their pacemaker's functionality or potential pacemaker damage when exposed to electrosurgical equipment. If any uncertainty arises, consult the cardiology department.
- Electrosurgical equipment emits high-frequency energy radiation that can affect other medical devices, unrelated electronics, telecommunications systems, and navigation systems. To prevent interference, you must maintain a minimum distance of at least 1.5 meters between the electrosurgical equipment and other devices.
- Regularly inspect accessories, with special attention to electrode cables and any endoscopy accessories, to ensure there is no damaged insulation or other defects that could compromise their safety or effectiveness.
- To connect accessories compatible with the equipment's characteristics, you must compare the insulation characteristics of the accessories (information provided by the manufacturers) with the specifications of the supplied unit (as outlined in the Technical Characteristics section). This step ensures proper compatibility and safe operation.
- **Caution:** Equipment failure could lead to an inadvertent increase in power output.
Note: Stimulation of the patient's muscles or nerves may be caused by low-frequency currents resulting from electrical sparking between the electrodes and the patient's tissue. If neuromuscular stimulation occurs during surgery, take the following steps:
 1. Pause the surgery immediately.
 2. Thoroughly inspect all connections to the generator to identify any potential issues or loose connections.
 3. If the problem persists and cannot be resolved through connection checks, it is imperative to have the generator inspected by qualified personnel for necessary maintenance and troubleshooting.

INSTALLATION

- Electrical safety is guaranteed only when the equipment is correctly connected to a reliable power supply network with proper grounding, in compliance with current safety standards. It is essential to ensure this fundamental safety requirement, and if there are any doubts, seek a comprehensive inspection of the system by qualified personnel. The manufacturer cannot be held responsible for potential damage caused by the absence of an efficient earth connection in the installation. Operating the equipment without a protective earth connection is strictly prohibited.
- Before connecting the equipment, verify that the provided voltage, as indicated on the rear panel, matches the voltage available in your mains power supply.
- In the event of any incompatibility between the power socket and the equipment's power cable, only replace it with a suitable type. It is not allowed to use adapters, multiple connections, or extension cables. If their use becomes necessary, it is mandatory to employ single or multiple adapters that comply with current safety standards.
- Protect the equipment from exposure to outdoor elements such as rain and direct sunlight. The apparatus must be shielded to prevent the infiltration of liquids.
- Do not keep the equipment plugged in unnecessarily. Turn it off when it is not in use to conserve energy and ensure safe operation.
- This equipment is not designed for use in explosive environments. Avoid using it in such environments where there may be a risk of ignition or explosion.
- The equipment should be used only for its intended purpose. Any other use should be considered improper and potentially dangerous. The manufacturer cannot be held responsible for any damage resulting from improper, incorrect, or unreasonable use.
- Modifying or attempting to modify the equipment is dangerous and should not be done. Altering the characteristics of the equipment can lead to unsafe operation and potential hazards.
- Before performing any cleaning or maintenance procedure, disconnect the appliance from the electrical supply by either unplugging it from the mains or turning off the main switch of the system.
- In the event of equipment breakage or malfunction, power it off immediately. For any necessary repairs, seek assistance only from an authorized service center and request the use of original spare parts. Failure to adhere to these regulations may jeopardize equipment safety and pose risks to the user.
- Do not reduce or disable the acoustic signal indicating generator activation. A functioning activation signal can help minimize or prevent injuries to patients or personnel in the event of accidental activation.
- Do not test the equipment's operation by generating power between the active and neutral electrode or between the active electrode and metal parts. Testing in this manner can be unsafe.
- If required, use appropriate fume extraction methods in the surgical field to manage the release of smoke or fumes generated during procedures.

PATIENT SAFETY

During high-frequency electrosurgery procedures, it's crucial to understand that the patient becomes a conductor of electrical voltage relative to the earth potential. Consequently, if there is contact between the patient and electrically conductive objects (such as metal objects, damp or wet sheets, cloths, etc.), it can result in the generation of electric current at the point of contact.

It is allowed to conduct thorough inspections of the device and its accessories before use, and to strictly adhere to all pertinent safety regulations.

CORRECT PATIENT POSITIONING

Prevent any deliberate or accidental contact between the patient and grounded metal components by ensuring the following:

- The patient does not come into contact with metal parts such as the operating table or supports.
- Ensure that respirator hoses do not rest on the patient's body.
- Always maintain coatings on the grounded operating table to dissipate electrostatic charges.
- Place the patient on a thick fabric with insulating properties, covered with an adequate number of layers.
- Ensure the patient does not touch damp sheets or mattresses.
- Prevent body secretions, cleaning fluids, or other liquids from soaking dry sheets.
- Keep the area beneath the patient free of liquid residue.
- Employ catheters to manage urinary excretions.
- Keep areas of the body prone to increased sweating or areas with skin-to-skin contact points dry using drapes (e.g., arm/body trunk, leg/leg, breasts, skin folds).
- Properly insulate all conductive and grounding supports and brackets.
- Adjust the anesthesia dosage to prevent excessive sweating.

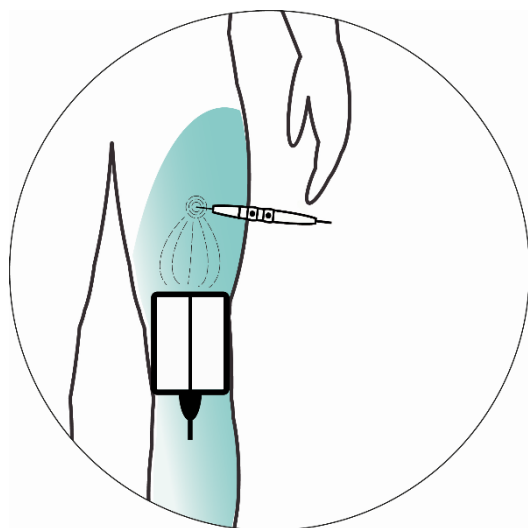
CORRECT APPLICATION OF THE NEUTRAL ELECTRODE

In monopolar electrosurgery, the use of a neutral electrode, also known as a current leakage plate, is essential. It facilitates the safe return of the cutting or coagulation current to the electrosurgical unit. There are two types of neutral electrodes:

1. **Monopolar Neutral Electrode:** In this type, there is no control over the contact between the neutral electrode and the patient.
2. **Bipartite Neutral Electrode:** This type offers control over the contact between the neutral electrode and the patient.

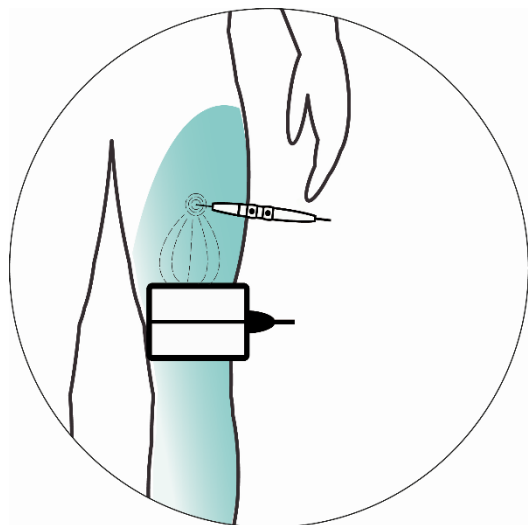
Ensuring the correct placement of the neutral electrode is of utmost importance to prevent burns and minimize patient risks. Below are some valuable tips to achieve this:

1. *Correct positioning*



In the image alongside, the correct positioning of the split neutral electrode is illustrated. The patient-plate should be placed perpendicular to the surgical field. Avoid positioning it transversely and instead, prefer a vertical or diagonal orientation. This promotes a uniform distribution of the current over the surface of the neutral electrode, minimizing the risk of burns to the patient.

2. *Incorrect Positioning*



In the image alongside, the incorrect positioning of the split neutral electrode is illustrated. The parallel arrangement between the patient-plate and the surgical field causes a non-uniform distribution of current across the two surfaces of the neutral electrode, potentially leading to alarm notifications on the unit and preventing the correct activation of the device.

For both single-part and dual-part electrodes, before proceeding with the placement of the neutral electrode, clean and remove any residues of foreign substances from its surface.

Do not apply the neutral electrode on scars, bony prominences, or anatomical areas where prosthetic implants or monitoring electrodes are present. Instead, apply it on well-irrigated tissues, such as muscles and in proximity to the surgical site.

If a disposable neutral electrode is being used, adhere to the expiration dates. If a reusable neutral electrode is used, ensure that the fastening systems provide stability.

It is of paramount importance that the neutral electrode is firmly applied over its entire surface to prevent burns. When a neutral electrode partially detaches from the patient, the current density in the remaining electrode area increases. As the current density beneath the neutral electrode becomes uneven, non-uniform heating occurs, especially at the edges of the neutral electrode.

If the electrode were placed in an area subjected to pressure during the procedure, the compressive load would result in reduced skin perfusion. Consequently, the generated heat can only be partially dissipated, thereby increasing the risk of burns. Furthermore, there is an increased risk of pressure points (decubitus) formation due to the heating that occurs. This temperature rise leads to a higher demand for oxygen (O₂) and energy in the affected area, contributing to the potential development of pressure areas on the body.

HIGH-FREQUENCY ELECTROSURGERY IN LAPAROSCOPY

Laparoscopic surgery, or minimally invasive surgery, has revolutionized the field of surgical procedures, bringing significant benefits in terms of patient recovery times and healing. In this context, the use of high-frequency monopolar surgery (HF) is widely employed due to its flexibility in performing cuts, coagulations, and mixed cuts that combine both functions. However, this surgical approach carries risks for the patient, especially the risk of burns.

The risks of burns can be exacerbated by various factors, including limited visual field, inadequate maintenance of laparoscopic equipment, interference on the monitor, insufficient surgeon preparation or distractions, excessive smoke development, inadequate insulation, capacitive currents, and accidental contact of the active electrode tip with surrounding tissue. These factors can contribute to an increased risk of burns, internal injuries, tissue necrosis, and organ perforation.

Furthermore, within the surgical environment, where the active electrode closely interacts with conductive instruments and bodily tissue, there are factors that can promote the transfer of electrical currents to concealed areas. These factors include:

1. **Direct Coupling:** This occurs when the active electrode makes contact with another metal instrument, leading to the transmission of electrical current and an increased risk of burns to nearby tissue, such as the intestines or other organs.
2. **Insulation Failure:** In this case, the insulation surrounding the electrode can become compromised due to excessive voltage, improper use, or damage to the electrode shaft. This can happen during surgery or during the cleaning and sterilization of instruments. An invisible insulation breakdown,

when the electrode is activated, poses a risk of unpredictable and potentially more insidious burns. Surprisingly, a minor insulation breakdown can be more hazardous than a major one, as it concentrates the current, making burns more likely.

3. **Capacitive Coupling:** This occurs when the active electrode induces electrical current in conductive materials, even if the insulation remains intact. During high frequency electrosurgery, the rapid changes in the electric field around the active electrode are only partially hindered by insulation, generating ionic currents that, upon contact with tissue, can cause sufficient heating to induce burns.

Addressing these risks with great care and implementing preventive measures is crucial to ensuring patient safety during high-frequency surgery in a laparoscopic setting.

To minimize the risk of burns during high frequency electrosurgery procedures in laparoscopy, consider the following preventive measures:

- **Comprehensive Staff Training:** Provide thorough and meticulous training for medical and healthcare personnel involved in electrosurgery procedures. It is essential to ensure they have a complete understanding of the procedures, associated risks, and preventive measures.
- **Detailed Inspection of Surgical Instruments:** Conduct a meticulous visual examination of surgical instruments, including the active electrode and laparoscope. This can help identify any defects or wear that could increase the risk of burns.
- **Use of Disposable Electrodes:** Although disposable electrodes may have thinner insulation that does not necessarily reduce the risk of insulation breakdown or capacitive coupling, they are free from wear and tear.
- **Avoidance of Hybrid Material Cannulas:** Steer clear of using cannulas made of hybrid materials, such as plastic and metal, as they can heighten the risk of direct coupling and capacitive coupling.
- **Adoption of Bipolar Technique:** While the bipolar technique may be less versatile than the monopolar one, it is considered safer because heat injuries are localized and occur only with prolonged current application.

In conclusion, burns are a genuine concern in high frequency electrosurgery procedures. However, with a deep understanding of potential causes and thorough preparation of the medical team, it is possible to limit their occurrence and effectively manage potentially risky situations.

PUTTING INTO SERVICE

- **Inspect the Equipment for Shipping Damage:** Check the equipment for any damage caused during shipping. If you find any damage, please report it immediately to the carrier and document the damage found. You should also inform LED SpA or your seller. When returning the equipment, use the original packaging or packaging that ensures safe transport.
- **Unpack and Review the Documentation:** Carefully remove the appliance from its packaging and study the provided documentation and operating instructions. Ensure that the mains voltage, as indicated on the nameplate data, matches the local mains voltage (mains frequency: 50-60Hz). If necessary, replace the fuses with the values specified on the data plate.
- **Connect to a Grounded Power Socket:** Connect the power cord to a mains socket with a reliable earth connection.

USING THE EQUIPMENT WITHOUT PROPER GROUNDING IS STRICTLY PROHIBITED.

- **Ensure Proper Installation:** The equipment must be placed on a flat surface with dimensions at least corresponding to the base of the equipment. Leave a minimum of 25 cm of space around the equipment.
- **Connect Mains Cable:** Attach the mains cable to the power socket located on the rear panel of the unit.
- **Establish Equipotential Connection:** Connect the equipotential connection point on the rear left side of the unit to the equipotential socket of the system.
- **Connect Pedal or Footswitch (Optional):** If you have a pedal or double footswitch (optional), connect it to the corresponding connector on the front panel of the unit.
- **Connect Handpiece:** If you are using a handpiece with buttons, connect it to the appropriate connection points. If you are using a handpiece without buttons, it must be connected to the "active" socket.
- **Operate in a Suitable Environment:** Ensure that the equipment is used only in a dry environment. Any condensation that forms must be allowed to evaporate before operating the equipment. Adhere to the ambient temperature and humidity levels, and do not exceed the specified limits.
- **Environmental conditions:**

	OPERATION	TRANSPORT / STORAGE
Temperature:	from 10 to 40 °C	from -10 to 50 °C
Relative Humidity:	from 30% to 75%	from 10 to 100%
Atmospheric Pressure:	from 70 to 106 kPa	from 50 to 106 kPa

- **Upon Activation:** When turning on the equipment using the switch located on the rear panel, the device will start with the function and power levels used during the last activation.
- **Monopolar Mode:** In monopolar mode, it is essential to connect the neutral electrode cable to the corresponding neutral electrode. If a split neutral electrode is used, ensure that the circuit is properly closed (connected correctly to the patient). This action will cause the red indicator light on the neutral electrode connector to stop flashing if the impedance value is acceptable.
- **Before Using the Equipment:** Before attempting to use the equipment, it is necessary to connect the patient plate cable. When using split electrodes, close the circuit by connecting the electrode to the patient. If the impedance value read by the equipment is acceptable, the OC indicator light will stop flashing, and you will receive an audible signal to indicate proper functionality.

CONNECTORS AND CONTROLS

LABEL ON REAR PANEL

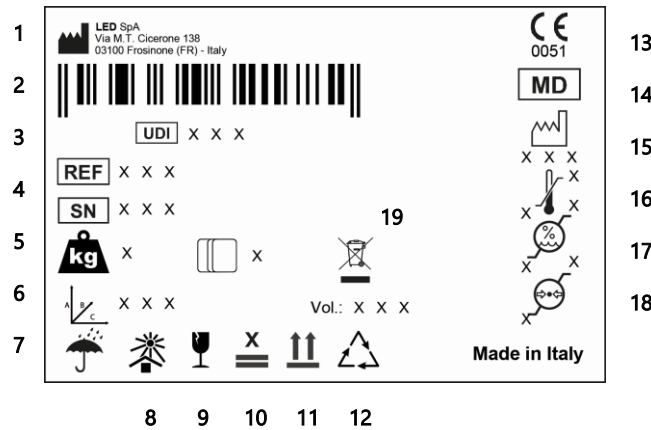
Safety requirements for high-frequency (HF) surgical equipment necessitate the clear printing of data and symbols on the cabinet, or at the very least, on one of the panels of the power unit. These data and symbols serve a crucial role in defining the equipment's characteristics and monitoring its operational conditions to guarantee safe and effective utilization of the device.

MEANING OF GRAPHIC SYMBOLS

N°	SYMBOL	DESCRIPTION
1		Floating neutral electrode: not connected to ground at either high or low frequencies.
2		CF Class equipment protected against defibrillator-induced discharge.
3		Non-ionising radiation generator equipment.
4		Follow the instructions for use.
5		CE Mark (2017/745/EU) + Notified Body Number 0051 = IMQ Italy.
6		The product should not be disposed of in urban waste containers but must be disposed of through separate collection.
7		Manufacturer.
8		Serial Number.
9		Production date.
10		Unique Device Identification.
11		Medical Device.
12		Dealer.
13		No maintenance by the user.
14		Catalogue number (Code).
15		Temperature Limits.
16		Humidity Limits.
17		Atmospheric Pressure Limits.
18		This Way Up.
19		FRAGILE – Handle With Care.
20		Keep away from sunlight.
21		Protect against moisture.
22		Number of maximum stackable packages.
23		Weight.
24		Dimensions.
25		Number of Pieces.
26		Recycle.
27		Model/Trade Name.
28		Protection against harmful ingress of water or particulate matter.
29		Fuse.

BOX LABEL

With reference ISO15223-1 "Medical Devices-Symbols to be used with medical device, labels, labelling and information to be supplied" and ISO780 "Packaging – Pictorial marking for handling of goods" on box label of UNIT's carton box are present these indications:



- | | |
|--|---|
| 1. ISO15223-1 (5.1.1) MANUFACTURER | 12. ISO 7001: 2007 RECYCLING (Indicates the location of a bin or container) |
| 2. ISO15223-1 (5.7.10) UDI code = EAN code | 13. CE + Notified Body Number for MD Class (2017/745/UE) |
| 3. ISO15223-1 (5.1.6) CATALOGUE NUMBER | 14. ISO15223-1 (5.7.7) MD (Medical Device) |
| 4. ISO15223-1 (5.1.7) SERIAL NUMBER | 15. ISO15223-1 (5.1.3) DATE OF MANUFACTURER |
| 5. WEIGHT OF BOX | 16. ISO15223-1 (5.3.7) TEMPERATURE LIMITS (Indicates temperature limits within which the transport package shall be stored and handled) |
| 6. DIMENSIONS OF BOX | 17. ISO15223-1 (5.3.8) HUMIDITY LIMITS (Indicates humidity limits within which the transport package shall be stored and handled) |
| 7. ISO15223-1 (5.3.4) KEEP DRY (Transport package shall not be kept from moisture) | 18. ISO15223-1 (5.3.9) ATMOSPHERIC PRESSURE LIMITS (Indicates atmospheric pressure limits within which the transport package shall be stored and handled) |
| 8. ISO15223-1 (5.3.2) KEEP AWAY FROM SUNLIGHT (Transport package shall not be exposed to sunlight) | 19. WEEE PRODUCT (Directive 2012/19/EU) |
| 9. ISO15223-1 (5.3.1) FRAGILE (Contents of the package are fragile therefore it shall be handled with care) | |
| 10. STACKING LIMIT BY NUMBER (Indicates the maximum number of identical products that can be safely stacked on the bottom package) | |
| 11. ISO780 (3) THIS WAY UP (Indicates correct upright position of the transport package) | |

FRONT PANEL



1. USB PORT

To perform software updates, use the USB 2.0 port located on the front of the unit.

2. TOUCHSCREEN DISPLAY

The backlit LCD touchscreen display allows for the visualization and selection of all set and adjustable parameters within a specific procedure.

3. MONOPOLAR OUTPUT CONNECTORS

This is the connection point for the handpiece with dual buttons to activate cutting (CUT) and coagulation (COAG) functions. If handpieces without buttons or optional monopolar cables are used, they should be connected to the socket labeled "ACTIVE."

4. NEUTRAL ELECTRODE CONNECTOR

This is the connection point for the neutral electrode to be applied to the patient. Disposable or reusable, single-part or split neutral electrodes can be used.

5. BIPOLAR OUTPUT CONNECTORS

This is the connection point for bipolar accessories.

6. POWER ON/OFF BUTTON

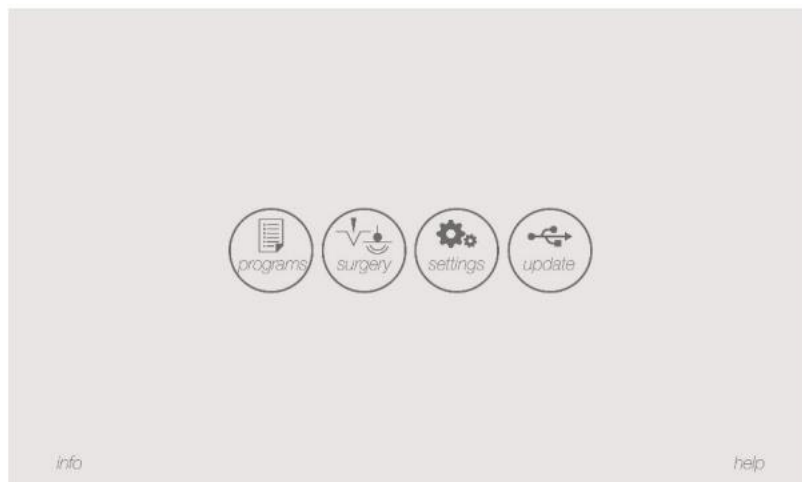
On the front panel, there is a button to turn on and off the device.

OPERATING MODES

CONTROL AND POWER ON

The unit is operated directly through the icons displayed on the touchscreen of the device. To confirm a selection, simply touch the icon.

Once the electrosurgical unit is powered on, the specific software begins to load on the screen. The progress of the software application process is indicated by the filling of the bar at the bottom of the screen. At the end of this process, the home screen will be displayed:



On the home screen, you can select and interact with the following options:

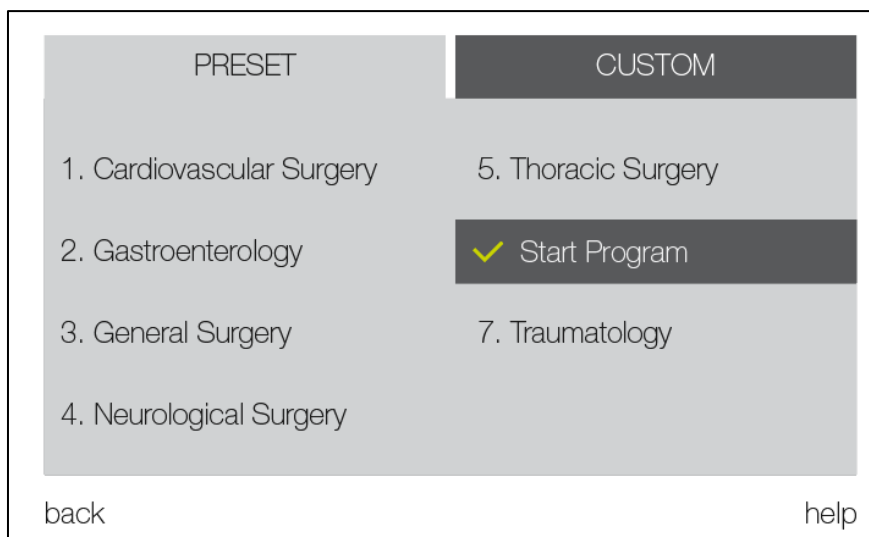
- Programs
- Surgery
- Settings
- Update (Software Update via USB Port).

Using the "*info*" option, you can view the currently installed software versions. By pressing the "*help*" button, you can access an informative summary that is helpful for correctly interpreting the indications displayed on the screen.

PROGRAMS

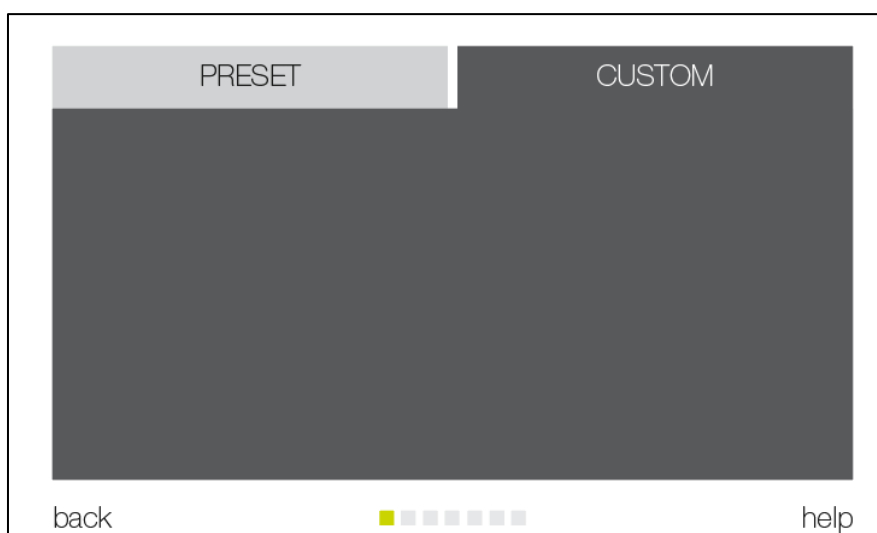
By selecting the *"Programs"* option on the home screen, two separate pages will open:

1. **Preset:** In this section, pre-configured programs that have already been set up and stored in the system will be displayed. These represent standard settings for a variety of common surgical procedures.



Simply click *"Start Program"* to activate the pre-set program and make it ready for use.

2. **Custom:** On this page, you will see programs that have been created and customized by the user or surgeon. These programs reflect specific settings that the user has configured to address particular needs or unique procedures.



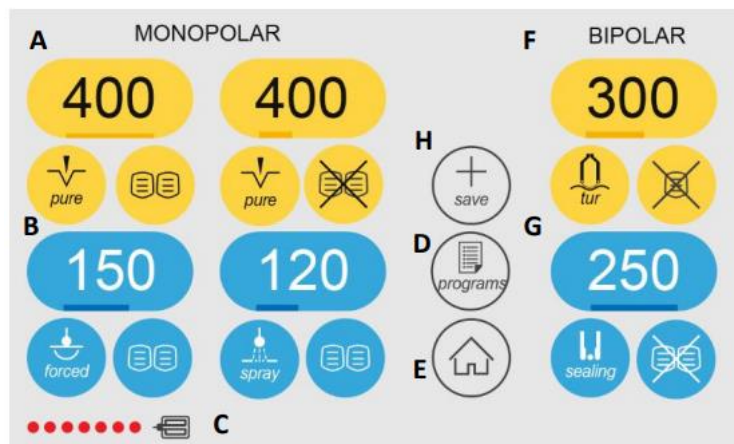
At first, the screen will appear empty. For instructions on how to create a personalized program, please refer to the next section (*"Programs Section"*).

The distinction between these two pages allows operators to easily access a range of predefined or customized settings, depending on the specific requirements of the surgical procedure. This provides flexibility in selecting settings according to the context.

Furthermore, by pressing '*Help*' on the display, you can obtain information about the features of the selected program. To return to the home page, simply select the '*Back*' option.

SURGERY

When selecting the '*Surgery*' option on the home page, the following screen will be displayed:



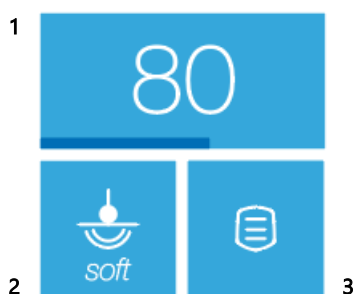
Through this screen, you can access different sections:

- A. Monopolar Sections Cut
- B. Monopolar Sections Coagulation
- C. Neutral electrode circuit impedance indication
- D. Program Section
- E. Home icon
- F. Bipolar Cut section
- G. Bipolar section Coagulation
- H. New Program Storage

Each of these options allows you to adjust various parameters, which can be saved as a new customized program.

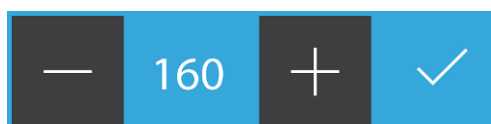
MONOPOLAR SECTION

In the sections dedicated to adjusting cutting or coagulation, both in monopolar and bipolar modes, there are three icons:



1. *Icon for adjusting the output power*

By tapping the icon with the number, you can adjust the output power. Below is an example to illustrate the procedure:



Pressing the '+' and '-' buttons adjusts the power, while pressing the '✓' button confirms the selected value.

2. *Icon to select the deliverable current*

By tapping the icon with the function, you can select the desired one.

CUT CURRENT (CUT)



The ideal current for cutting is pure sinusoidal without modulation, i.e., with a 100% duty cycle.

BLENDED CURRENT (BLEND)



The blended current (BLEND) is suitable for coagulated cutting when you want to achieve deep coagulation combined with cutting. Its waveform has a lower modulation percentage compared to pure coagulation. This current consists of a sinusoidal current component suitable for cutting, combined with a low-voltage coagulation current (SOFT COAG). This creates a current that is suitable for coagulated cutting without the formation of eschar or charring and is particularly suitable for endoscopic procedures.

ENHANCED CUT CURRENT (ENHANCED CUT)



The enhanced cut current (ENHANCED CUT) is a sinusoidal current characterized by amplitude modulation and is suitable for cutting tissues, particularly adipose tissues.

TRANS URETHRAL RESECTION CURRENT (TUR CUT)



The TUR current, when used with a specific bipolar accessory, is suitable for both cutting and coagulated cutting when a deliberate coagulation effect is desired in addition to the cutting action. This current is generated by adapting a sinusoidal current for cutting, combined with a high-voltage coagulation current.

DUPLICATE CUT CURRENT (DUO CUT)



The DUO CUT function is set on both connected handpieces. It is possible to perform the same function simultaneously on both handpieces.

FORCED COAG CURRENT (FORCED COAG)



The modulated current (FORCED COAG) has good surface coagulative properties but may also lead to the potential formation of eschar and slight tissue carbonization. The advantage of this type of coagulation lies in the speed at which the desired effect is achieved.

FORCED COAG is also referred to as Speedy.

DUPLICATE COAGULATION CURRENT (DUO COAG)



The DUO COAG function is set on both connected handpieces. It is possible to deliver the same function simultaneously on both handpieces.

SOFT COAG CURRENT (SOFT COAG)



The low-voltage, low modulation current (SOFT COAG) is suitable for coagulating deep tissue layers, where cellular albumin coagulation is achieved without carbonization or eschar formation. The coagulation process in this case is slower than in FORCED COAG coagulation.

SOFT Coag is also referred to as Pin Point, Dessicate, or Deep.

FULGURATION COAGULATION CURRENT (FULGURATE)



The high-voltage fulguration coagulation current (FULGURATE) is directed into the active electrode that is not in contact with the tissue being treated and is primarily responsible for coagulation. This method is ideal for treating large surfaces with widespread and superficial bleeding (e.g., liver resection) and/or for achieving coagulation at the open sternum level in cardiac surgery.

SPRAY COAGULATION CURRENT (SPRAY COAG)



The SPRAY COAG high-voltage current passes through the active electrode, which does not make direct contact with the targeted tissue but primarily induces a coagulation effect. This technique is particularly well-suited for treating extensive areas with diffuse and superficial bleeding, such as in liver resection or for coagulation during open sternum procedures in cardiac surgery.

ARGON CURRENT FOR SPRAY COAGULATION WITH ARGON (SPRAY ARGON)



A compatible external Argon unit must be connected.

Argon is an inert gas that is used to achieve a coagulating effect on patient tissue. The gas contained in the cylinder is delivered at low pressure in the direction of the tissue, while a function with a suitable output voltage is activated to trigger the Argon spark and thus initiate the coagulation process (without contact between the active electrode and the tissue), which is extremely effective and useful not only in traditional open surgery, such as liver resections, but also in laparoscopic and endoscopic surgery.

3. *Icon for activating the footswitch*

By tapping the icon with the footswitch, you can choose which one to activate, for example:



Footswitch Activated



Footswitch Not Activated

Using the optional footswitch with the selector:



Footswitch Activated



Footswitch Not Activated

BIPOLAR SECTION

In the bipolar section, just like in the monopolar section, you can adjust the output power, select the deliverable current, and activate the footswitch. The difference lies in the mode-specific selectable functions for each mode. You will need to connect the bipolar accessories to the connectors for this function and use the pedal switch.

BIPOLAR CUT CURRENT (BIPOLAR CUT)



The current supplied by bipolar forceps is a high-voltage pure sinusoidal current suitable for cutting without coagulation.

TRANS URETHRAL BIPOLAR RESECTION CURRENT (BIPOLAR TUR)



The TUR current, using a specific bipolar accessory, is suitable for both cutting and coagulated cutting when forced coagulation along with cutting is desired. This current consists of a sinusoidal current component suitable for cutting, along with a high-voltage current component for coagulation.

MICRO CUT



The current supplied to the bipolar accessory operates at a low voltage to ensure a more controlled and precise cutting action. This function is ideal for microsurgery applications.

BIPOLAR COAG CURRENT (BIPOLAR COAG)



This type of coagulation is achievable with bipolar forceps and allows for the delivery of radiofrequency output power at low impedances, such as those typically encountered in the tissue section that can be positioned between the tips of the forceps.

BIPOLAR TUR COAGULATION CURRENT (BIPOLAR TUR COAG)



The BIPOLAR TUR COAG current, when utilized with a dedicated bipolar accessory, is effective for both cutting and coagulated cutting when deliberate coagulation along with cutting is required. This current is generated by combining a sinusoidal current adjusted for cutting with a high-voltage coagulation current.

MICRO COAG



The current provided to the bipolar forceps is low-voltage, allowing for controlled and precise coagulation of small blood vessels. This function is well-suited for microsurgical procedures.

VESSEL SEALING



This type of function is suitable for arterial and venous vascular synthesis and coagulation using radiofrequency clamping. The vessel is gently clamped with slight pressure, radiofrequency is initiated, and pressure with the forceps is maintained until coagulation occurs.

For the operation of the bipolar modes, please refer to the "AUTOSTART AND AUTOSTOP" section.

AUTOSTART AND AUTOSTOP

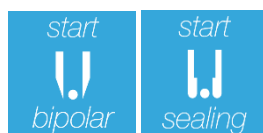
In the Bipolar functions, you can access four different operating settings:

- **No preset output automation**



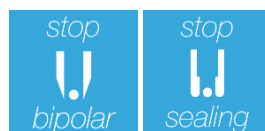
The output is only activated by pressing the pedal and stops when released.

- **START**



To activate the "*start bipolar*" or "*start sealing*" function, you need to press the pedal, establish contact between the active electrode and the tissue, and this will activate the output. If you wish to stop, simply release the pedal.

- **STOP**



To activate the "*stop bipolar*" or "*stop sealing*" function, you need to press the pedal; the output is activated (even if there is no contact between the tissue and the active electrode) and stops when the tissue is coagulated or if the pedal is released.

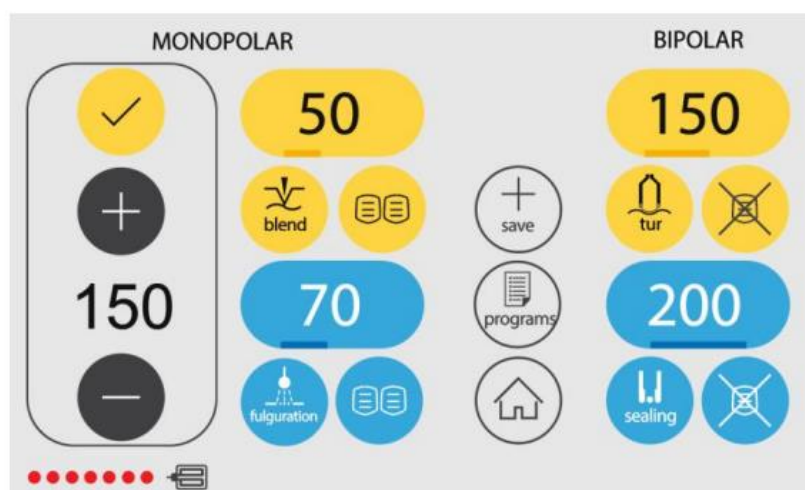
- **AUTOSTART/AUTOSTOP**



To activate the "*start/stop bipolar*" or "*start/stop sealing*" function, you need to press the pedal, establish contact between the active electrode and the tissue, and this will activate the output. The output stops when the tissue is coagulated or if the pedal is released.

DISPENSING SCREEN

In the dispensing state, the screen will display the function along with its respective level. This screen remains for a few seconds during which you can adjust the output level using the + and - buttons.



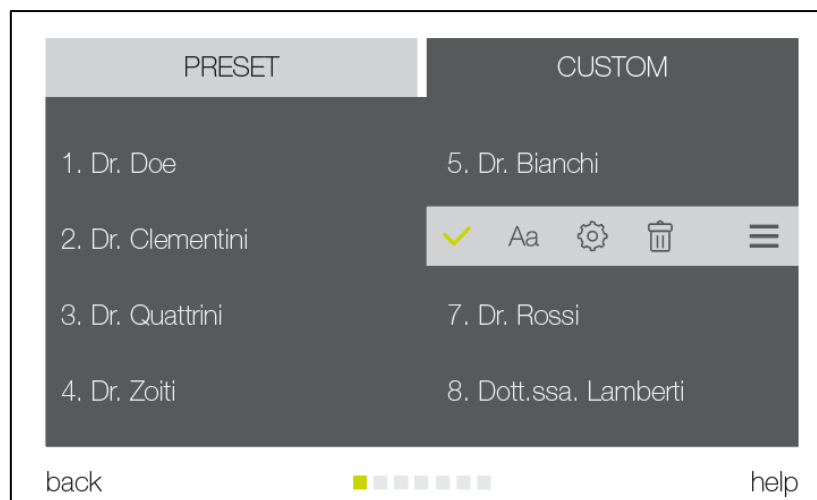
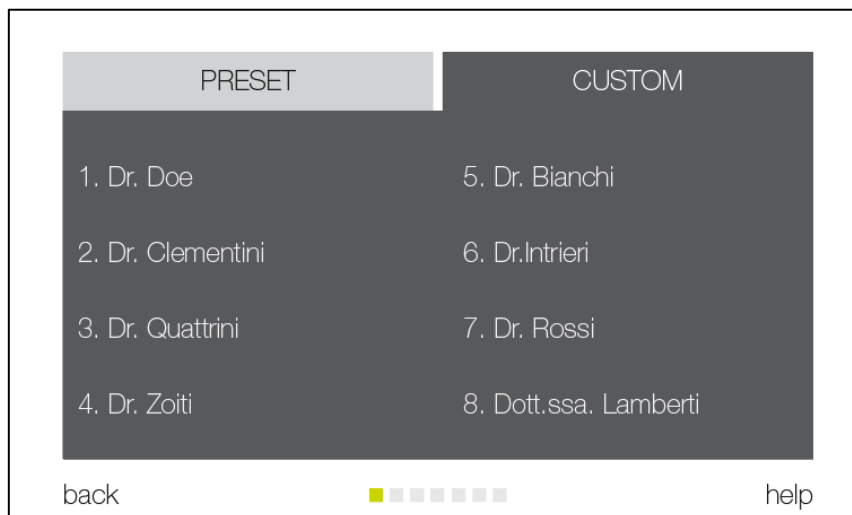
PROGRAMS SECTION

In the *"Surgery"* screen, you can add a custom program or view the existing programs.

To create a new program, follow the following procedure:

- Set the desired values in the 'Surgery' screen.
- Press '+' and choose the name to assign, completing the process by clicking 'enter'.

The new customized programs can be viewed in the 'Programs' section.





Through the icon representing three lines, you can perform various actions on the customized program:



Rename it.



Modify it.



Delete it.

NEUTRAL ELECTRODE CONTROL

The neutral electrode circuit is continuously monitored by a special circuit. This circuit checks, especially when bipartite neutral electrodes are in use, for any loss of contact between the patient reference plate or changes in the conductivity characteristics of the neutral electrode. Such changes can lead to a reduction in circuit conductivity, increasing the risk of burns to the patient.

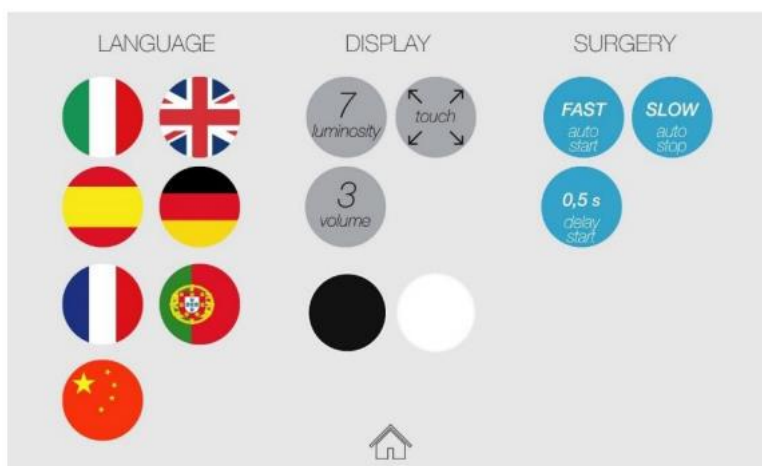


To reduce acoustic pollution, the audible alarm only triggers when the delivery pedal is held down.

It's important to note that when using single-section (single-part) neutral electrodes, the circuit only checks the connection of the neutral electrode to the unit. Therefore, it's crucial to ensure that the entire surface of the neutral electrode is correctly and securely applied to the patient.

SETTINGS

Starting from the home page and selecting the "*Settings*" option will bring up the following screen:



Through this screen, you will be able to access three sections:

- Language.
- Display, where you can adjust brightness, touchscreen sensitivity, volume, and switch between colour and black-and-white display.
- Surgery, which allows you to select the surgical intervention delay response and fast-medium-slow autostart/autostop.

With the start and autostart functions (see "AUTOSTART AND AUTOSTOP" section), you can select the delay time between contact between the active electrode and the tissue and the activation of the output (from 0.1 s to 2.0 s).

The sensitivity settings for autostart and autostop functions can be set to SLOW, MEDIUM, and FAST. Pressing the "home" icon will take you back.

UPDATE

Starting from the home page and choosing the "Update" option, you can update:

- Software
- Images
- Protocols
- Firmware

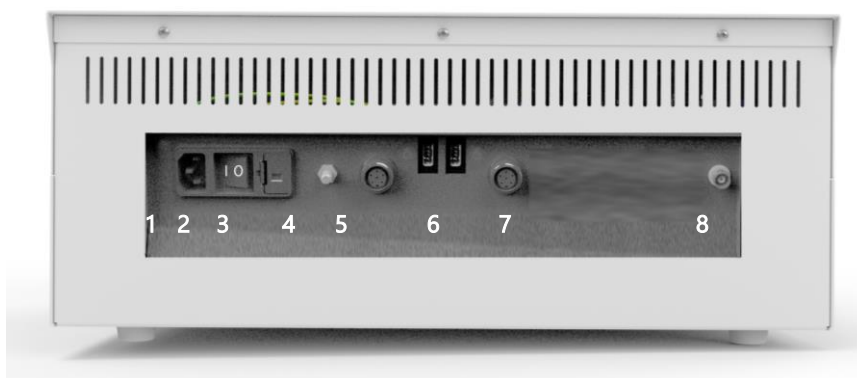


To perform updates, you need to connect a compatible device to the USB connector, which contains the compatible file for the software, images, protocols, or firmware to be updated. Follow these steps:

1. Insert the compatible device into the equipment's USB connector.
2. On the screen, select the corresponding option among "Software," "Images," "Protocols," or "Firmware."
3. Confirm the selection through the popup that appears.
4. Follow the on-screen instructions to complete the update process.
5. Once the update is complete, you can select the "Home" or "Back" option to exit the procedure and return to the main screen.

It is crucial to carefully follow the on-screen instructions throughout the entire process to ensure a correct and safe update.

BACK PANEL



1. Power supply socket
2. Power switch
3. Fuse Holder / Voltage Selector
4. Equipotential Socket
5. Bipolar Pedal Connector
6. USB sockets
7. Single-pole footswitch connector
8. External signal connector

POWER SUPPLY MODULE OF THE EQUIPMENT AND VOLTAGE SELECTOR

The equipment's power supply module serves as the connection point for supplying power to the internal electronics of the equipment. This power supply module includes the power connector and line fuses. The voltage selector is located inside the power supply module.

WARNING: Before powering on the equipment, the operator should ensure that the mains voltage indicated on the voltage selector matches the voltage it is connected to and that appropriate fuses for the selected voltage have been inserted.

POWER SWITCH

To turn on the power to the equipment, move the switch to position 1. When the power is on, the front panel will light up. Moving the switch to position 0 will turn off the power supply, serving as an emergency switch in case of any faults.

TECHNICAL CHARACTERISTICS

			DIATERMO MB 300 T	DIATERMO MB 400 T
	TOLERANCE	MONOPOLAR FUNCTIONS	TECHNICAL CHARACTERISTICS	
Function CUT <i>(pure)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	300 W - 300 Ω	400 W - 300 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	2500 Vpp	2500 Vpp
Function ENHANCED CUT <i>(enhanced)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	200 W - 300 Ω	250 W - 300 Ω
	± 5%	Modulation factor (Hz)	1.5/1.5/2.5/2.5/3.5/3.5	1.5/1.5/2.5/2.5/3.5/3.5
	± 0.3	Crest factor	3.3/3.2/3.1/3.0/2.8/2.6	3.3/3.2/3.1/3.0/2.8/2.6
	± 15%	Maximum output voltage	2500 Vpp	2500 Vpp
Function BLEND <i>(blend)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	200 W - 200 Ω	250 W - 200 Ω
	± 5%	Modulation factor	50 Hz	50 Hz
	± 0.3	Crest factor	2.4/2.8/2.7/2.6/2.5/2.4	2.4/2.8/2.7/2.6/2.5/2.4
	± 15%	Maximum output voltage	2500 Vpp	2500 Vpp
Function DUO CUT <i>(duo)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	150 W - 300 Ω	200 W - 300 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	2000 Vpp	2000 Vpp
Function TUR CUT <i>(tur)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	250 W - 300 Ω	300 W - 300 Ω
	± 5%	Modulation factor	50 Hz	50 Hz
	± 0.3	Crest factor	2.4	2.4
	± 15%	Maximum output voltage	2200 Vpp	2200 Vpp
Function FORCED COAG <i>(forced)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	120 W - 200 Ω	150 W - 200 Ω
	± 5%	Modulation factor	30 kHz	30 kHz
	± 0.3	Crest factor	3.4	3.4
	± 15%	Maximum output voltage	3300 Vpp	3300 Vpp
Function SOFT COAG <i>(soft)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	120 W - 200 Ω	150 W - 200 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	1200 Vpp	1200 Vpp
Function FULGURATION <i>(fulguration)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	80 W - 300 Ω	100 W - 300 Ω
	± 5%	Modulation factor	30 kHz	30 kHz
	± 0.3	Crest factor	3.8	3.8
	± 15%	Maximum output voltage	3200 Vpp	3200 Vpp
Function DUO COAG <i>(duo)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	80 W - 300 Ω	100 W - 300 Ω
	± 5%	Modulation factor	30 kHz	30 kHz
	± 0.3	Crest factor	3.8	3.8
	± 15%	Maximum output voltage	3200 Vpp	3200 Vpp
Function SPRAY COAG <i>(spray)</i>	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	100 W - 500 Ω	120 W - 500 Ω
	± 5%	Modulation factor	30 kHz	30 kHz
	± 0.3	Crest factor	4.3	4.3
	± 15%	Maximum output voltage	4200 Vpp	4200 Vpp

			DIATERMO MB 300 T	DIATERMO MB 400 T
	TOLERANCE	MONOPOLAR FUNCTIONS	TECHNICAL CHARACTERISTICS	
Function SPRAY ARGON (argon)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	100 W - 500 Ω	120 W - 500 Ω
	± 5%	Modulation factor	30 kHz	30 kHz
	± 0.3	Crest factor	4.3	4.3
	± 15%	Maximum output voltage	4200 Vpp	4200 Vpp
	TOLERANCE	BIPOLAR FUNCTIONS	TECHNICAL CHARACTERISTICS	
Function CUT (pure)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	150 W - 50 Ω	150 W - 50 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	1000 Vpp	1000 Vpp
Function TUR CUT (tur)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	300 W - 300 Ω	300 W - 300 Ω
	± 5%	Modulation factor	50 Hz	50 Hz
	± 0.3	Crest factor	1.8	1.8
	± 15%	Maximum output voltage	800 Vpp	800 Vpp
Function MICRO CUT (micro cut)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	50 W - 50 Ω	50 W - 50 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	700 Vpp	700 Vpp
Function COAG (bipolar)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	150 W - 50 Ω	150 W - 50 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	500 Vpp	500 Vpp
Function TUR COAG (tur)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	250 W - 25 Ω	250 W - 25 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	600 Vpp	600 Vpp
Function MICRO COAG (micro coag)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	50 W - 50 Ω	50 W - 50 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	200 Vpp	200 Vpp
Function VESSEL SEALING (sealing)	± 10%	Frequency	360 kHz	360 kHz
	± 20%	Maximum output power	250 W - 25 Ω	250 W - 25 Ω
	± 0.3	Crest factor	1.6	1.6
	± 15%	Maximum output voltage	600 Vpp	600 Vpp

TOLERANCE	DESCRIPTION	DIATERMO MB 300 T	DIATERMO MB 400 T
		TECHNICAL CHARACTERISTICS	
± 5%	Power supply	100-240 Vac	100-240 Vac
± 1%	Mains frequency	50/60 Hz	50/60 Hz
± 10%	Electrical input power	1000 VA	1000 VA
-	Touch screen (size (inch))	● (9")	● (9")
-	Applicable bipolar neutral electrode	●	●
-	Bipolar mode with AUTOSTART / AUTOSTOP possibility	●	●
-	Automatic impedance control	●	●
-	Integrated Argon module	●	●
-	Argon cylinders can be connected	2	2
-	Selectable minimum level	1	1
-	ARGON flow regulation	0.2 - 10 LPM	0.2 - 10 LPM
-	Maximum ARGON inlet pressure	3.5 bar (50.76psi)	3.5 bar (50.76psi)
-	ARGON inlet pressure	3.0 bar (43.5psi)	3.0 bar (43.5psi)
-	Maximum ARGON outlet pressure	2.0 bar (29psi)	2.0 bar (29psi)
-	Storage of working conditions	●	●
-	Step power unit for powers from 0W to 50W	●	●
-	Step power 10 for powers above 50W	●	●
± 0.5	Dimensions (mm)	450x170x400	450x170x400
± 10	Weight (kg)	16	16
-	5x20 fuses type DELAYED	2 x T10AL, 250V	2 x T10AL, 250V
± 10%	Input electric current (240Vac) (A)	5	5
± 10%	Input electric current (100Vac) (A)	10	10
-	Adjustable sound level (45dBA to 65 dBA)	●	●
-	Output power accuracy warning	●	●
-	Last setting memory	●	●
-	Working condition memory (CUSTOM)	50	50
-	Self-check	●	●
-	Electrical class (EN60601-1)	Class I Applied Part CF	Class I Applied Part CF
-	MDR Class 2017/745/EU	II b	II b
-	EN55011 (CISPR 11) Class (Class/Group)	2 / A	2 / A
-	IP Protection Class	IP32	IP32
-	Patient circuit	F	F
-	Duty cycle (action/pause) in seconds	10 / 30	10 / 30
-	Possibility to activate monopolar output (foot pedal or handpiece buttons)	Foot/Finger	Foot/Finger
-	Possibility to activate bipolar output	Footswitch or Autom.	Footswitch or Autom.
-	Defibrillation-proof	●	●
-	Equipotential socket	●	●
-	ABS and metal housing	●	●

● = PRESENT

HARDWARE REQUIREMENTS

Microcontroller	ARM Cortex M4
Clock Frequency	200 MHz
Flash	2048 KB
Ram	512 KB
SDRAM DDR2	512 MB
Nand Flash	1 Gb
Peripherals	UART, I2C, SPI, Watch-dog timer, USB2.0
Visual	Display touchscreen 7" 800x480 px

MAINTENANCE

GENERAL

There are no user-adjustable parts inside the equipment for calibration or service purposes. Opening the equipment casing voids the warranty. If repair or adjustment is necessary, the entire equipment should be sent to the LED SpA service center in APRILIA (LT), ITALY, along with a description of the issue. User maintenance primarily involves cleaning and sterilizing accessories and performing equipment checks before each use. Conducting functional and safety checks to verify parameters is the responsibility of specialized technical personnel.

CLEANING THE ENCLOSURE

Whenever possible, use only disposable accessories and dispose of them as special hospital waste. However, because some accessories may need to be reused, it is essential to thoroughly clean and sterilize them before each new use. Refer to the instructions for use (IFU) provided by the supplier of each reusable accessory for information on the maximum number of cycles and the type of sterilization required.

CLEANING AND STERILIZATION OF ACCESSORIES

If disposable non-sterile accessories are used, you must meticulously follow the Instructions for Use (IFU) provided by the manufacturer for the sterilization method and to dispose of them according to the currently applicable regulations.

In the case of reusable accessories, you must adhere to the maximum number of cycles and the sterilization method specified in the manufacturer's Instructions for Use for each accessory.

GUIDE TO TROUBLESHOOTING

If you encounter any problems, it's crucial to verify that the installation and accessory setup have been executed correctly. The error code shown on the seven-segment display, along with the description on the LCD display, can offer valuable insights for diagnosing and resolving the issue.

Problems	Probable Cause	Solution
The equipment does not power on.	There is an interruption or absence of the main power supply.	Please verify the connection of the main cable and replace any fuses with new ones of the appropriate type where necessary.
The Neutral Electrode alarm is consistently active.	There is an interruption or lack of contact in the neutral electrode circuit.	Check the connection of the cable to the neutral electrode. Replace the cable of connection of the neutral electrode.
The unit fails to respond to the activation command.	Possible causes for the issue could include a breakdown of the handpiece or pedal, or incorrect connections of these components.	Replace the handpiece or the pedal. Verify the connection of the handpiece or of the pedal.
Error Code 001.	Current delivery control is activated during the power-on process.	Disconnect the handpiece or the pedal and switch on the unit again.
Error Code 004.	Error in the data conversion circuit.	Call for Service.
Error Code 010.	Error in the output power activation circuit.	Call for Service.
Error Code 022.	Communication Error.	Call for Service.

REPAIRS

High-frequency cables or electrode handle cannot be repaired. Always replace a faulty part with a new one.

FUSE REPLACEMENT

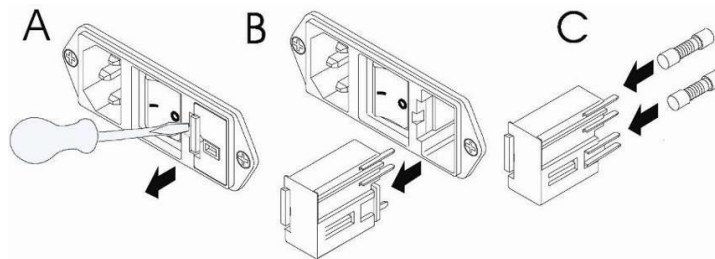
Before replacing the fuses, disconnect the equipment from the power supply.

For fuse replacement, use 5x20 type fuses and follow these steps:

(A-B) Using a small screwdriver, remove the fuse holder cartridges from the power module.

(C) Insert the fuses, referring to this information:

Voltage: 100-240 V Fuse Type: Time-Delay T10 AL, 250V / 5 x 20 mm



PRE-USE UNIT CHECK

Whenever the unit is scheduled for use, it is essential to perform a safety check, considering the following points:

- Inspect the integrity of cables, connections, wire breakage, etc.
- Ensure that all electrical equipment is properly grounded.
- Verify that all accessories to be used are available and sterilized.
- Check the operation of the OC light by disconnecting the reference electrode cable. Activate the unit and verify the OC light and audible alarm.
- Test the warning lights and audible signals by activating the CUT and COAG power switches.

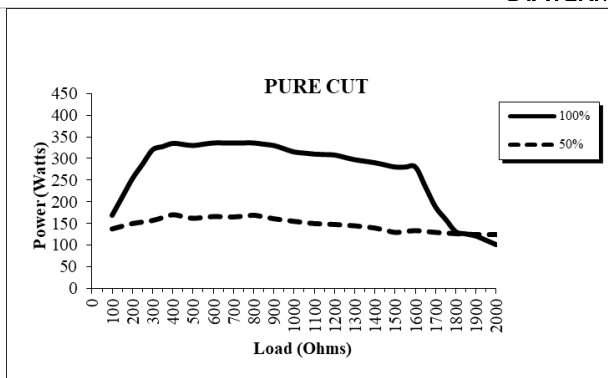
SAFETY AND MEASUREMENT FUNCTION CHECKS

Periodically (at least once a year), safety checks and measurements should be scheduled by the Department of Biomedical Engineering or other specialists. These include:

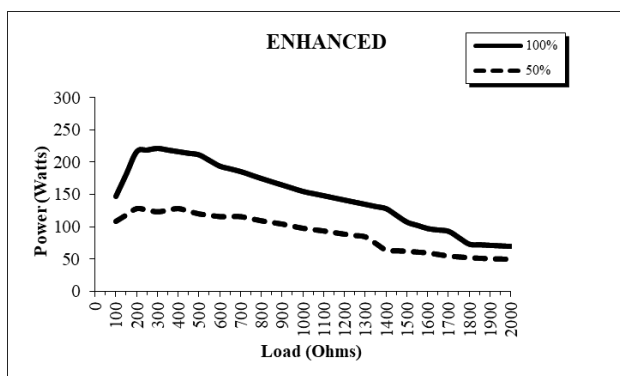
- Inspection of power cables and connectors.
- Visual inspection of mechanical protections.
- Evaluation of protections against hazards from liquid leakage, penetration, drips, humidity, hygiene products, and disinfectants.
- Review of data on the device panel.
- Verification of the availability of the instruction manual.
- Examination of high-frequency output.
- Measurement of grounding conductivity resistance.
- Measurement of high-frequency leakage current.
- Assessment of neuromuscular stimulation.
- Verification of output power correction.

DIAGRAMS

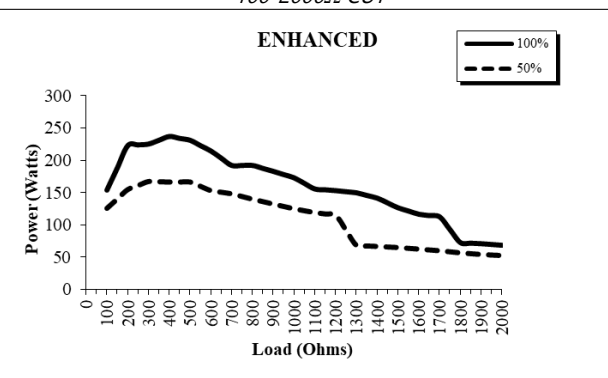
DIATERMO MB 300 T



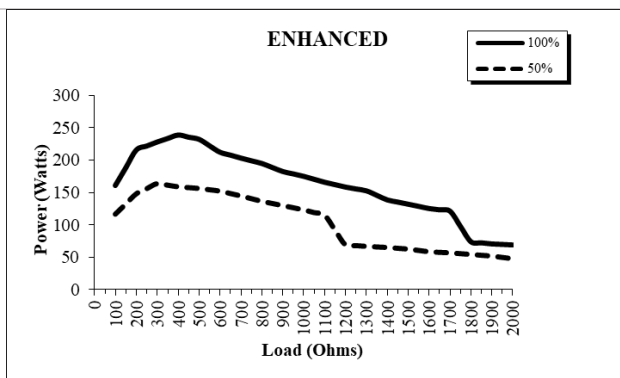
Diagrams of half and maximum output power versus impedance load 100-2000Ω CUT



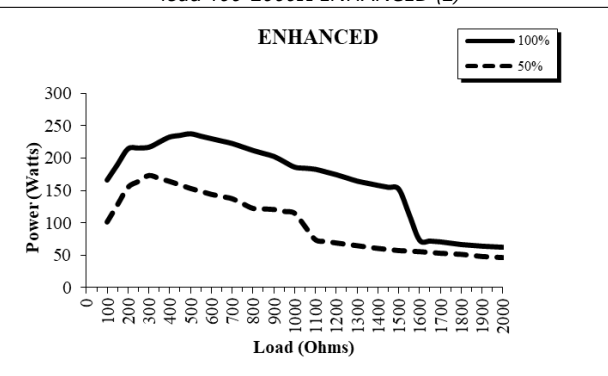
Diagrams of half and maximum output power versus impedance load 100-2000Ω ENHANCED (1)



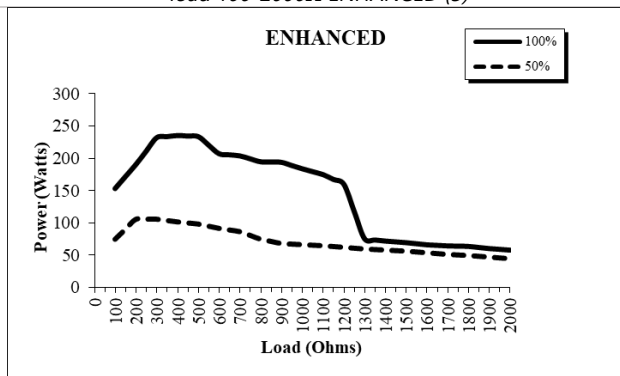
Diagrams of half and maximum output power versus impedance load 100-2000Ω ENHANCED (2)



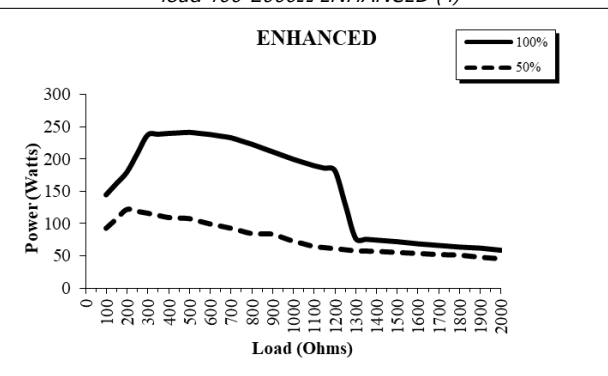
Diagrams of half and maximum output power versus impedance load 100-2000Ω ENHANCED (3)



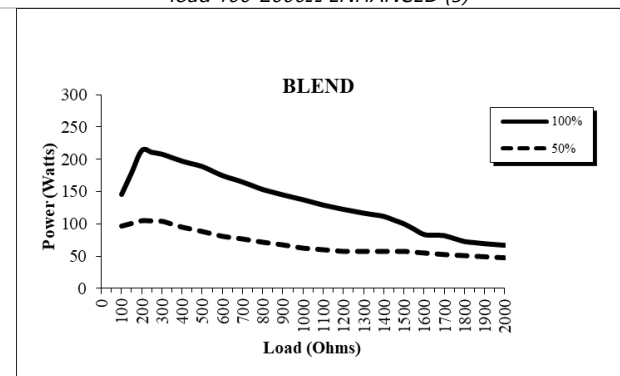
Diagrams of half and maximum output power versus impedance load 100-2000Ω ENHANCED (4)



Diagrams of half and maximum output power versus impedance load 100-2000Ω ENHANCED (5)

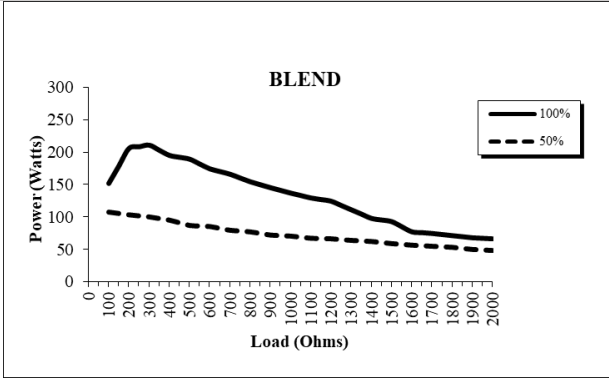


Diagrams of half and maximum output power versus impedance load 100-2000Ω ENHANCED (6)

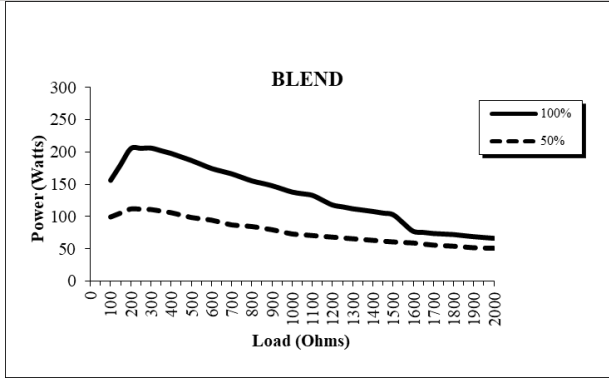


Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (1)

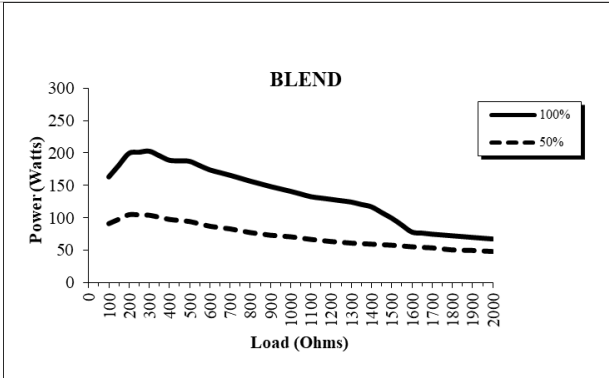
DIATERMO MB 300 T



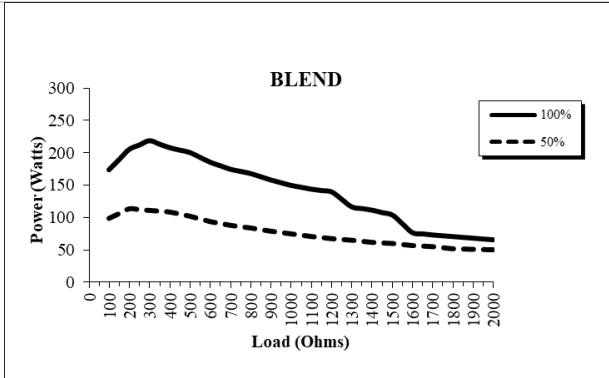
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (2)



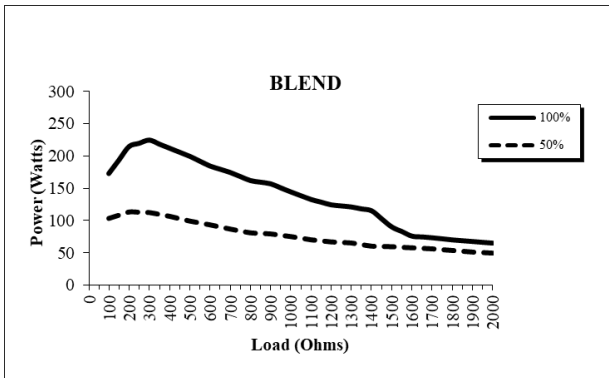
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (3)



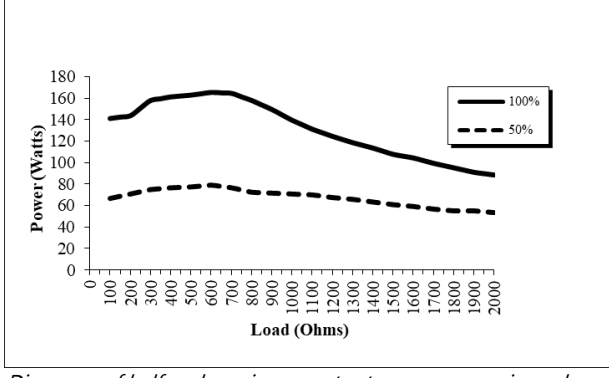
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (4)



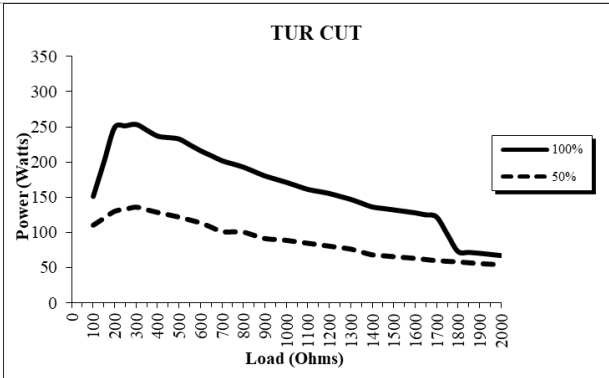
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (5)



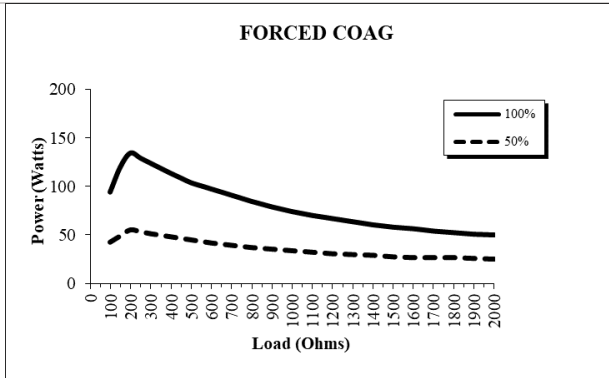
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (6)



Diagrams of half and maximum output power versus impedance load 100-2000Ω DUO

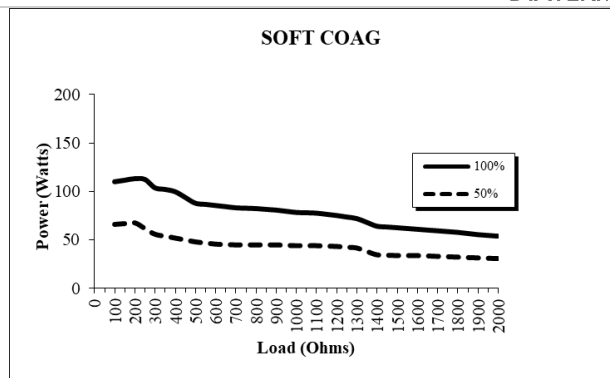


Diagrams of half and maximum output power versus impedance load 100-2000Ω TUR CUT

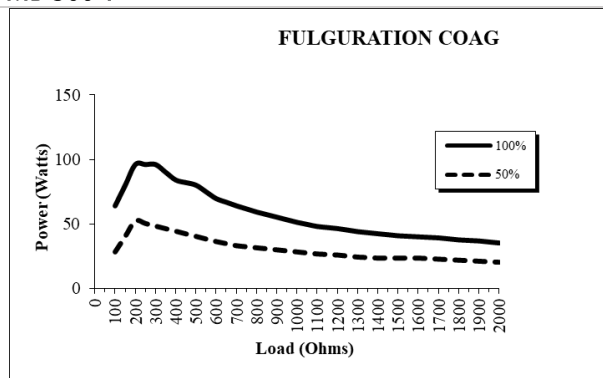


Diagrams of half and maximum output power versus impedance load 100-2000Ω FORCED COAG

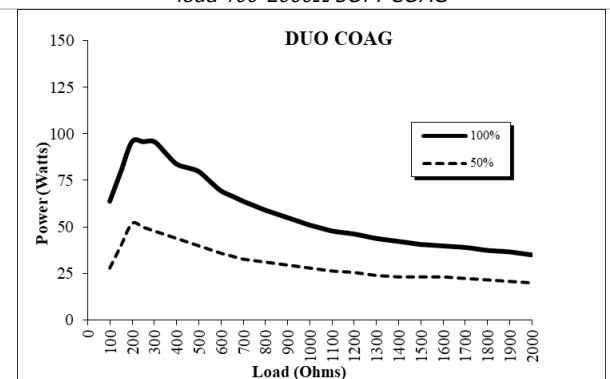
DIATERMO MB 300 T



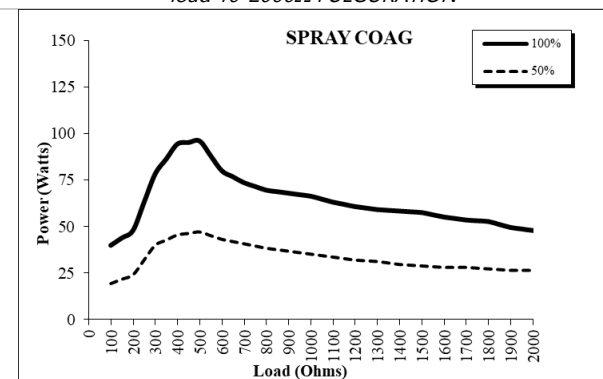
Diagrams of half and maximum output power versus impedance load 100-2000 Ω SOFT COAG



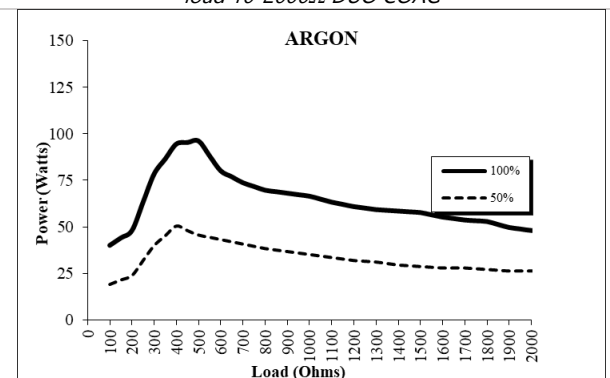
Diagrams of half and maximum output power versus impedance load 10-2000 Ω FULGURATION



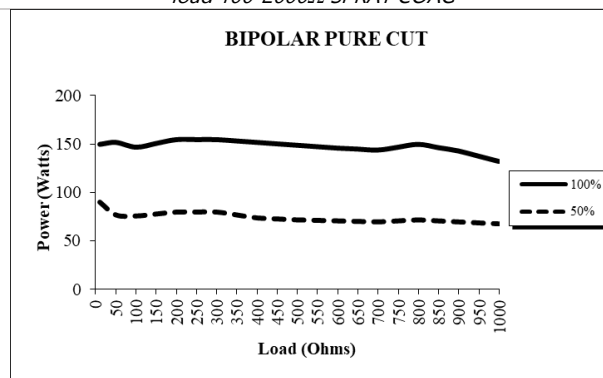
Diagrams of half and maximum output power versus impedance load 10-2000 Ω DUO COAG



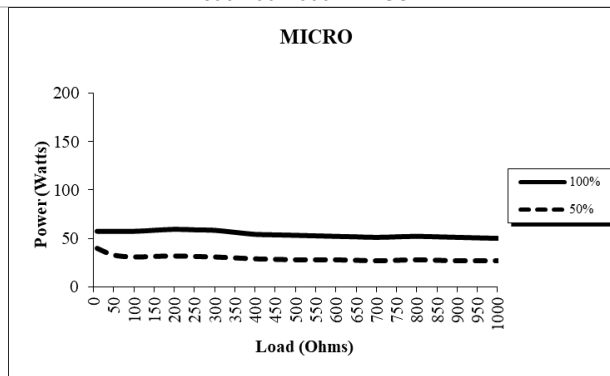
Diagrams of half and maximum output power versus impedance load 100-2000 Ω SPRAY COAG



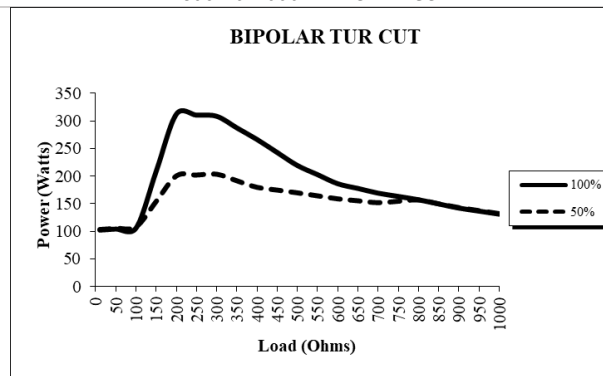
Diagrams of half and maximum output power versus impedance load 100-2000 Ω ARGON



Diagrams of half and maximum output power versus impedance load 10-1000 Ω BIPOLAR CUT

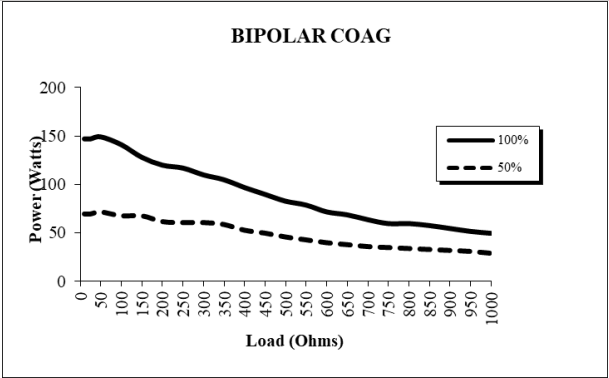


Diagrams of half and maximum output power versus impedance load 10-1000 Ω BIPOLAR MICRO CUT

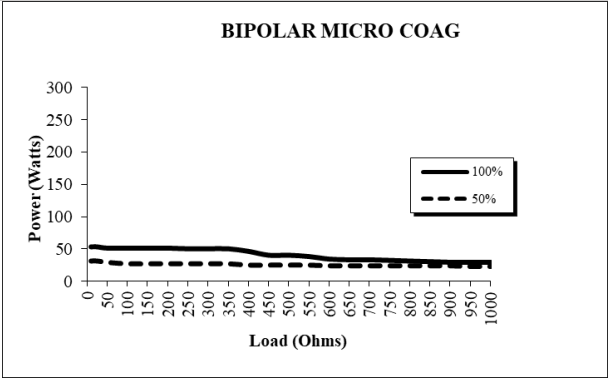


Diagrams of half and maximum output power versus impedance load 10-1000 Ω BIPOLAR TURCUT

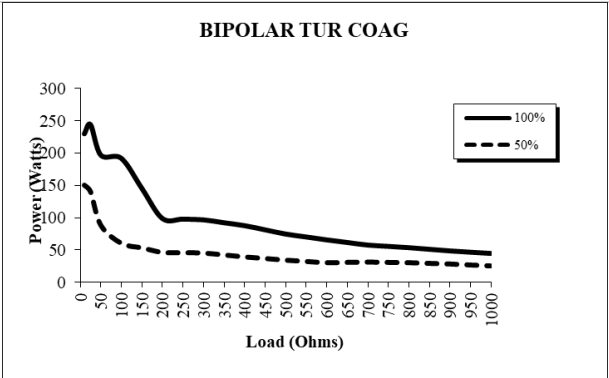
DIATERMO MB 300 T



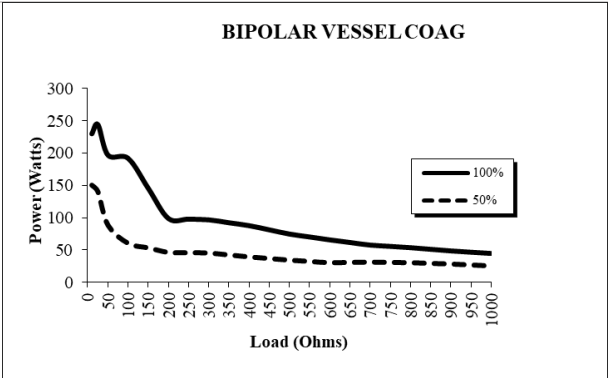
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR COAG



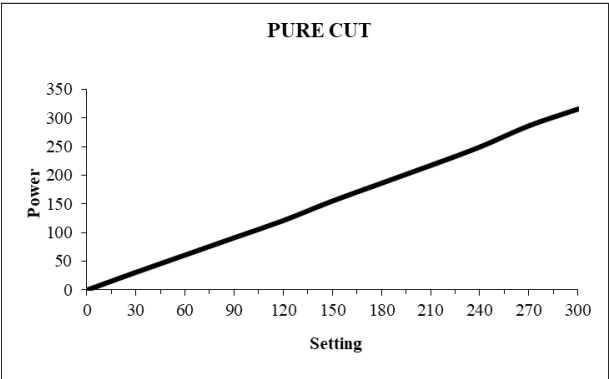
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR MICRO COAG



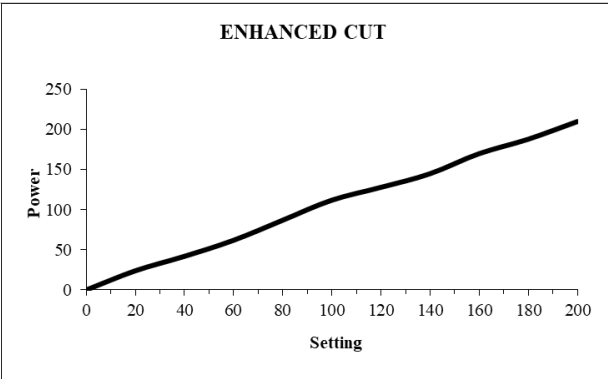
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR TUR COAG



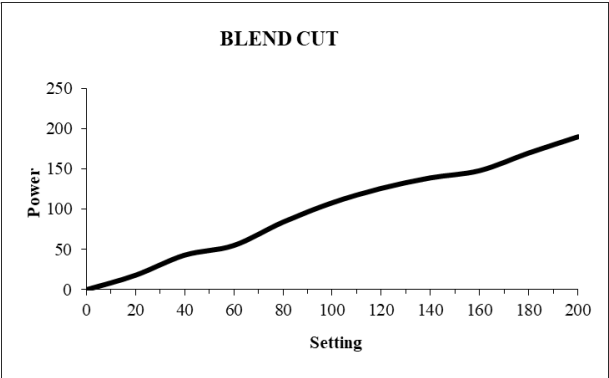
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR VESSEL



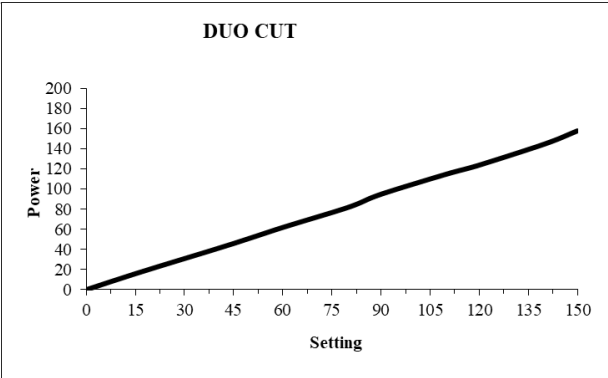
Diagrams of output power versus nominal value CUT100%



Diagrams of output power versus nominal value ENHANCED

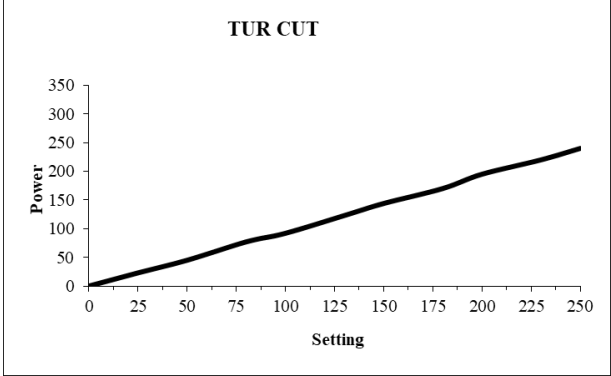


Diagrams of output power versus nominal value BLEND

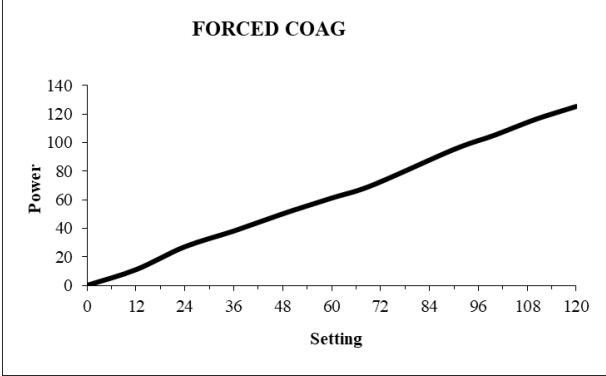


Diagrams of output power versus nominal value DUO CUT

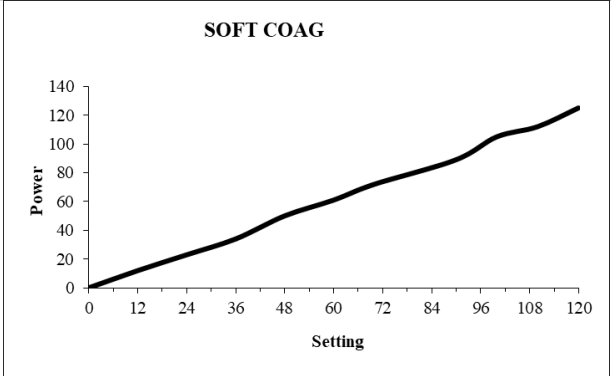
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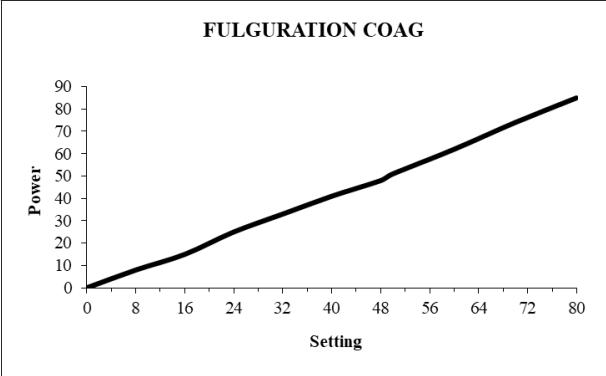
Diagrams of output power versus nominal value
TUR CUT



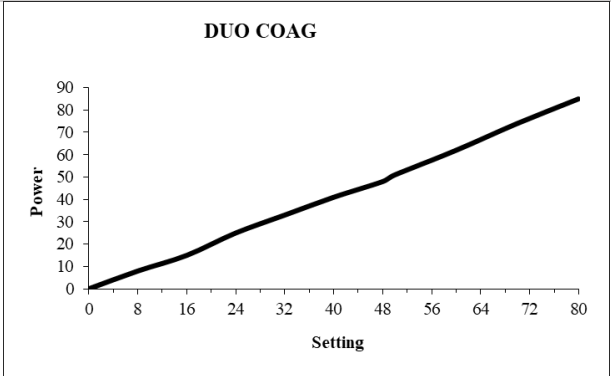
Diagrams of output power versus nominal value
FORCED COAG



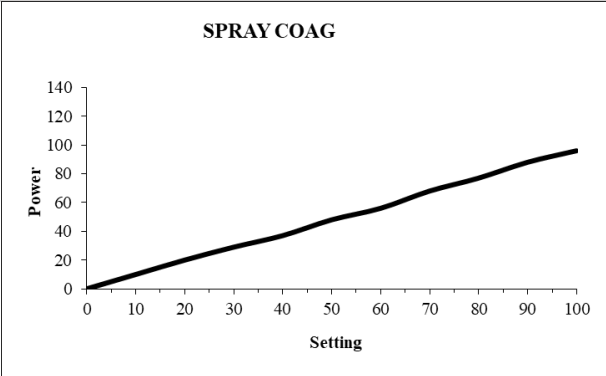
Diagrams of output power versus nominal value
SOFT COAG



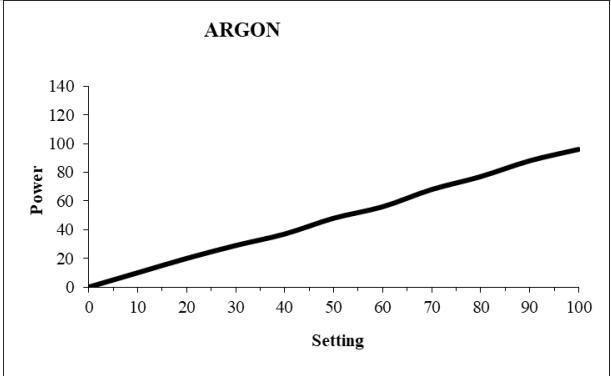
Diagrams of output power versus nominal value
FULGURATION



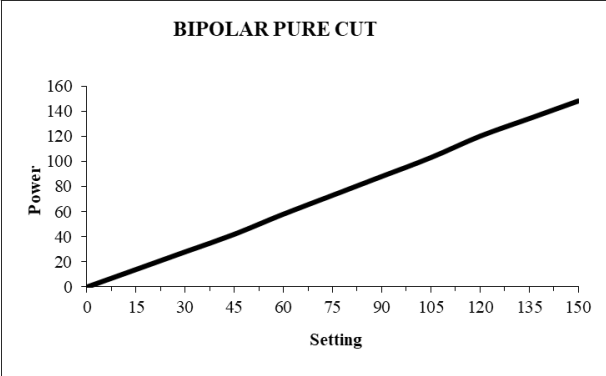
Diagrams of output power versus nominal value
DUO COAG



Diagrams of output power versus nominal value
SPRAY



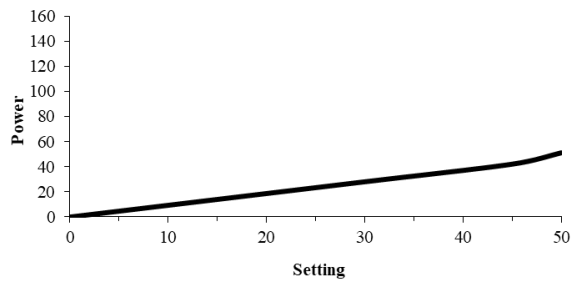
Diagrams of output power versus nominal value
ARGON



Diagrams of output power versus nominal value
BIPOLAR CUT

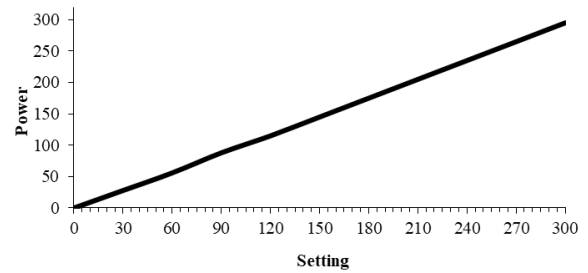
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BIPOLAR MICRO CUT



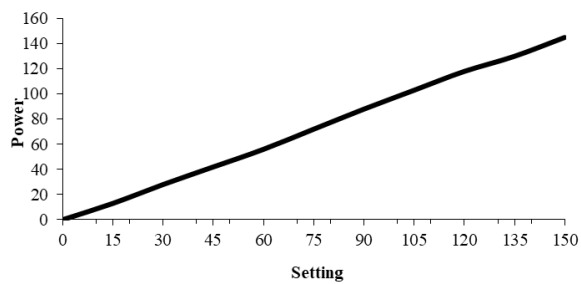
Diagrams of output power versus nominal value
BIPOLAR MICRO CUT

BIPOLAR TUR CUT



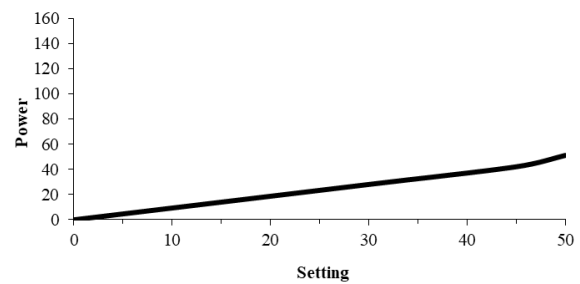
Diagrams of output power versus nominal value
BIPOLAR TURCUT

BIPOLAR COAG



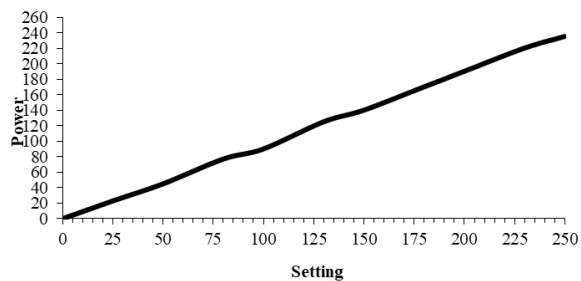
Diagrams of output power versus nominal value
BIPOLAR COAG

BIPOLAR MICRO COAG



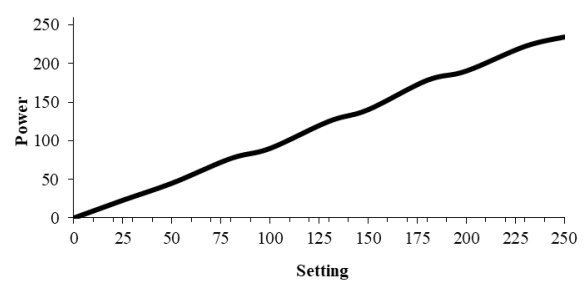
Diagrams of output power versus nominal value
BIPOLAR MICRO COAG

BIPOLAR TUR COAG



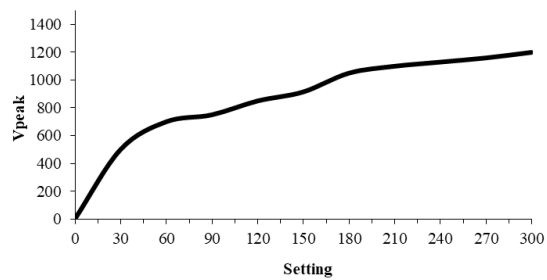
Diagrams of output power versus nominal value
BIPOLAR TUR COAG

BIPOLAR VESSEL SEALING



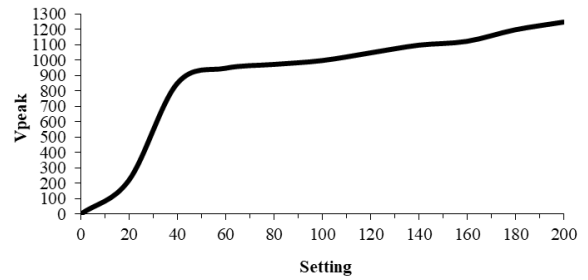
Diagrams of output power versus nominal value
BIPOLAR VESSEL

PURE CUT



Diagrams of maximum mains voltage output versus Vp
CUT 100%

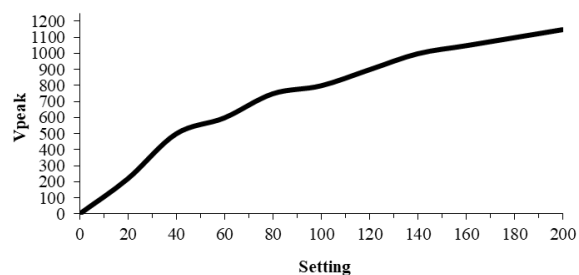
ENHANCED CUT



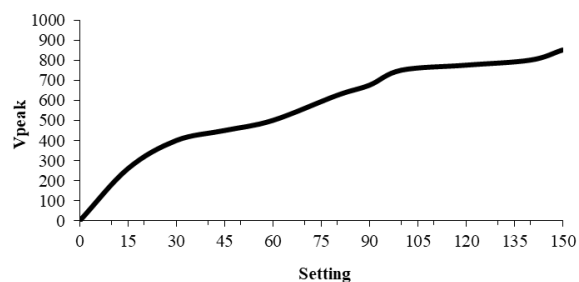
Diagrams of maximum mains voltage output versus Vp
ENHANCED

DIATERMO MB 300 T

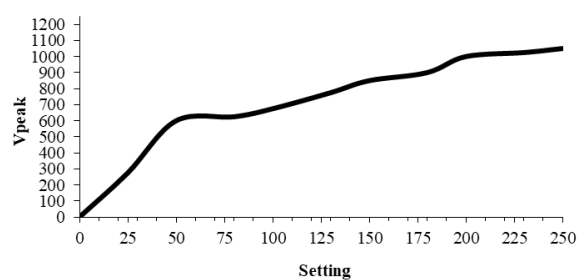
BLEND CUT

Diagrams of maximum mains voltage output versus Vp
BLEND

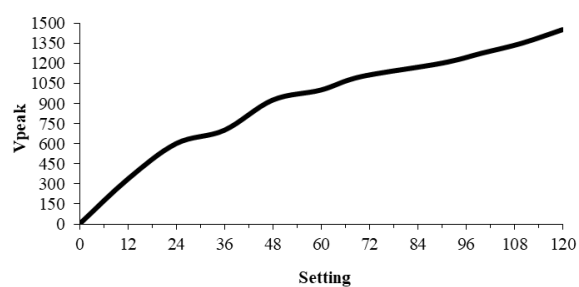
DUO CUT

Diagrams of maximum mains voltage output versus Vp
DUO CUT

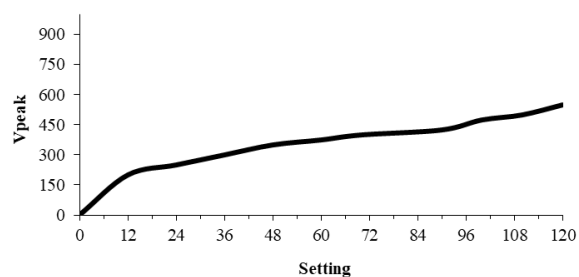
TUR CUT

Diagrams of maximum mains voltage output versus Vp
TUR CUT

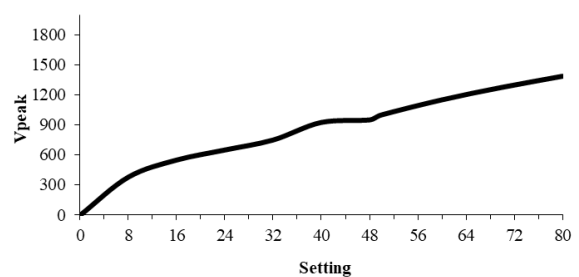
FORCED COAG

Diagrams of maximum mains voltage output versus Vp
FORCED COAG

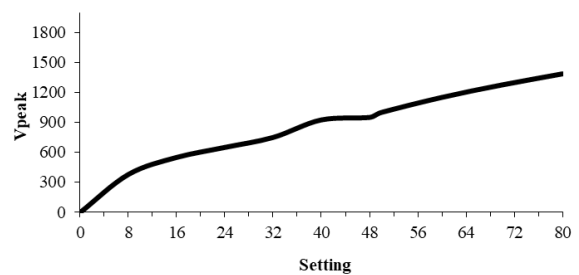
SOFT COAG

Diagrams of maximum mains voltage output versus Vp
SOFT COAG

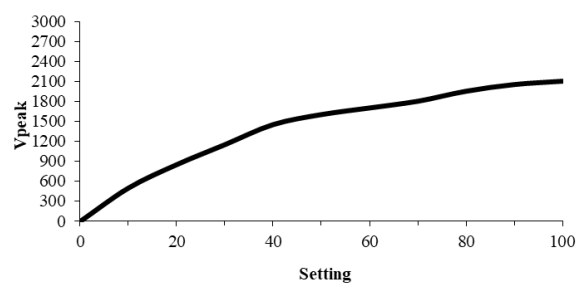
FULGURATION COAG

Diagrams of maximum mains voltage output versus Vp
FULGURATION

DUO COAG

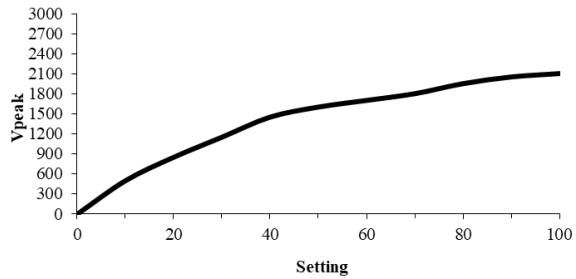
Diagrams of maximum mains voltage output versus Vp
DUO COAG

SPRAY COAG

Diagrams of maximum mains voltage output versus Vp
SPRAY

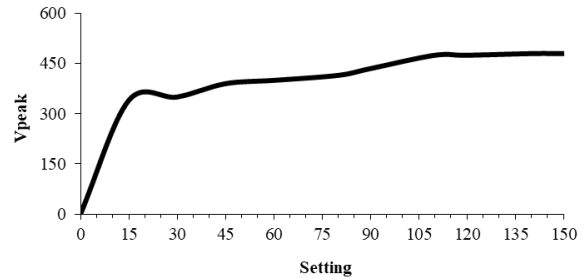
DIATERMO MB 300 T

ARGON



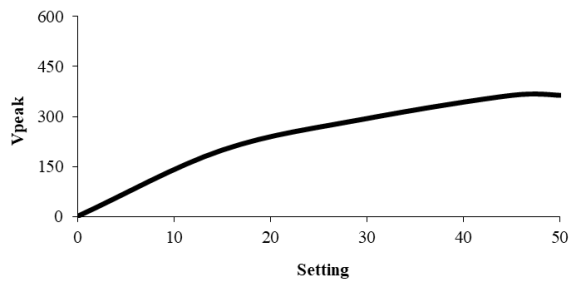
Diagrams of maximum mains voltage output versus Vp
ARGON

BIPOLAR PURE CUT



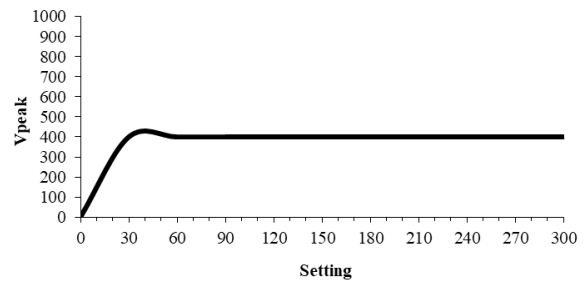
Diagrams of maximum mains voltage output versus Vp
BIPOLAR CUT

BIPOLAR MICRO



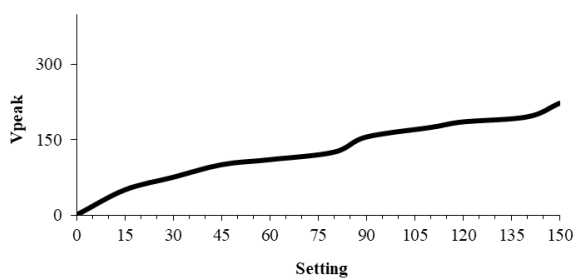
Diagrams of maximum mains voltage output versus Vp
BIPOLAR MICRO CUT

BIPOLAR TUR CUT



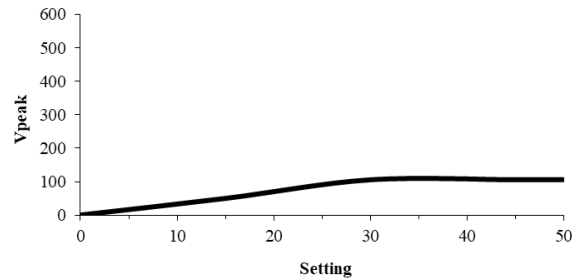
Diagrams of maximum mains voltage output versus Vp
BIPOLAR TUR

BIPOLAR COAG



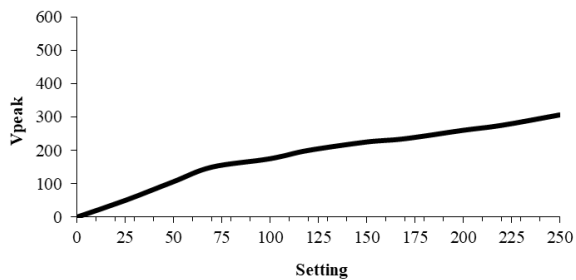
Diagrams of maximum mains voltage output versus Vp
BIPOLAR COAG

BIPOLAR MICRO COAG



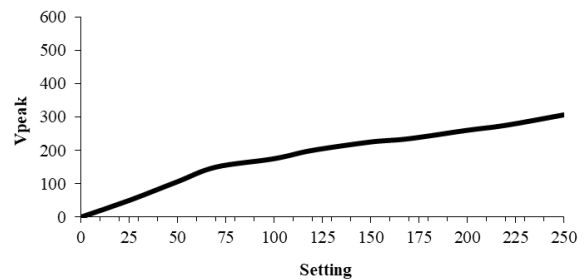
Diagrams of maximum mains voltage output versus Vp
BIPOLAR MICRO COAG

BIPOLAR TUR COAG



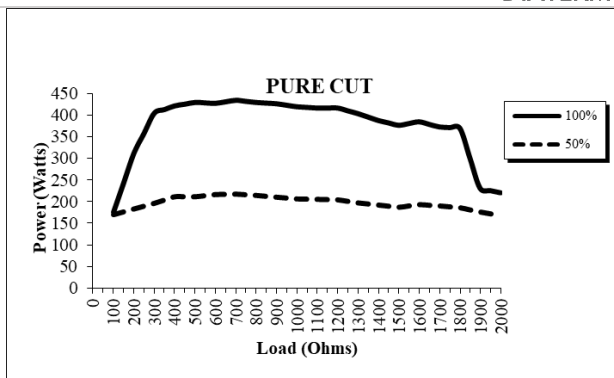
Diagrams of maximum mains voltage output versus Vp
BIPOLAR TUR COAG

BIPOLAR VESSEL SEALING

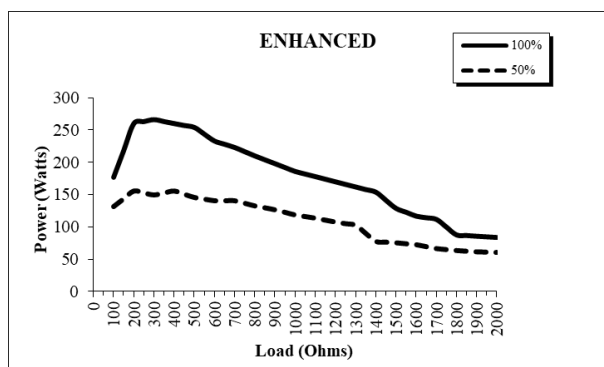


Diagrams of maximum mains voltage output versus Vp
BIPOLAR VESSEL

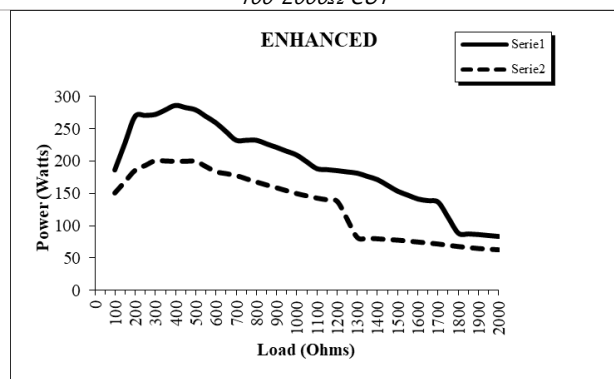
DIATERMO MB 400 T



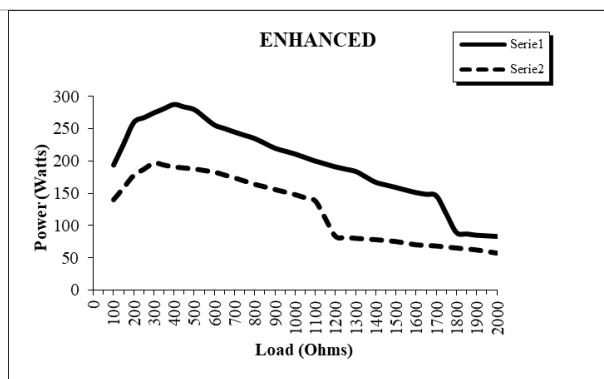
Diagrams of half and maximum output power versus impedance load
100-2000 Ω CUT



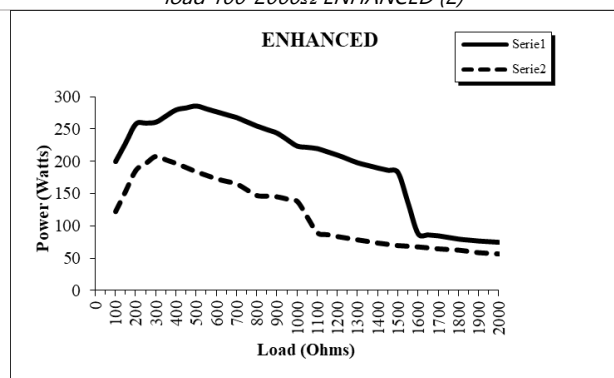
Diagrams of half and maximum output power versus impedance load 100-2000 Ω ENHANCED (1)



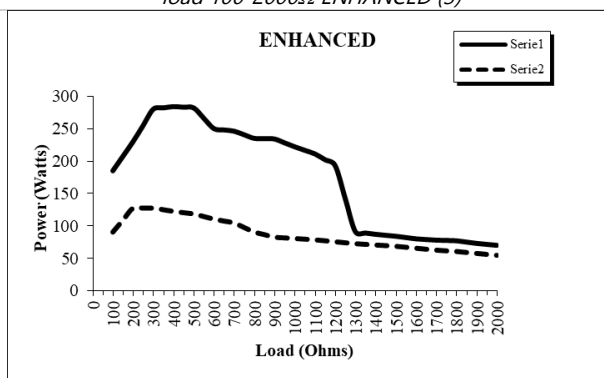
Diagrams of half and maximum output power versus impedance load 100-2000 Ω ENHANCED (2)



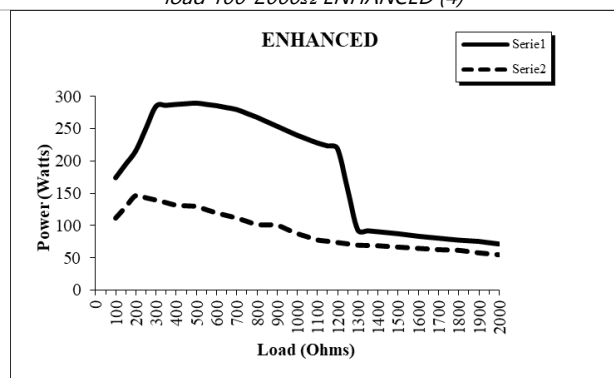
Diagrams of half and maximum output power versus impedance load 100-2000 Ω ENHANCED (3)



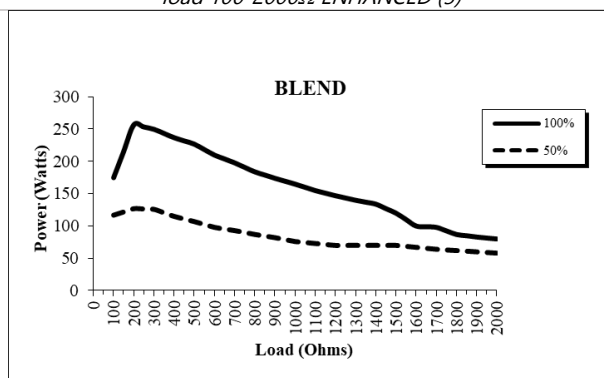
Diagrams of half and maximum output power versus impedance load 100-2000 Ω ENHANCED (4)



Diagrams of half and maximum output power versus impedance load 100-2000 Ω ENHANCED (5)

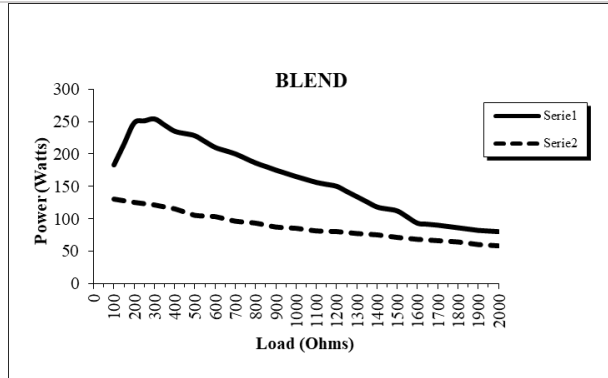


Diagrams of half and maximum output power versus impedance load 100-2000 Ω ENHANCED (6)

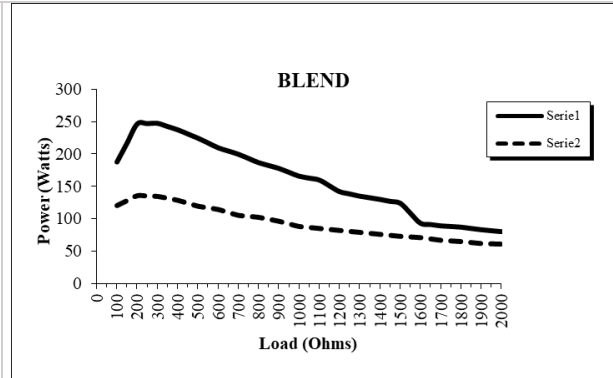


Diagrams of half and maximum output power versus impedance load 100-2000 Ω BLEND (1)

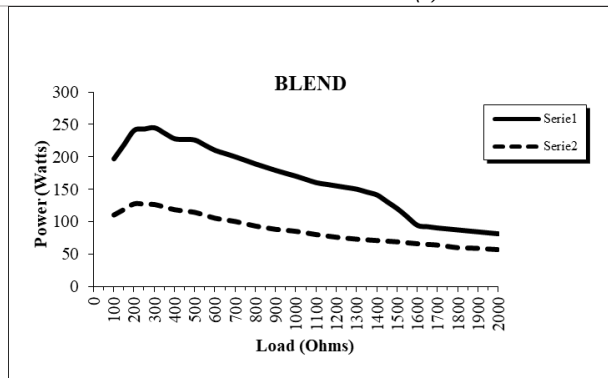
DIATERMO MB 400 T



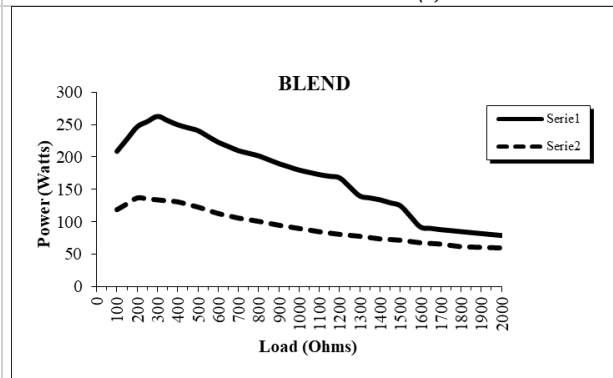
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (2)



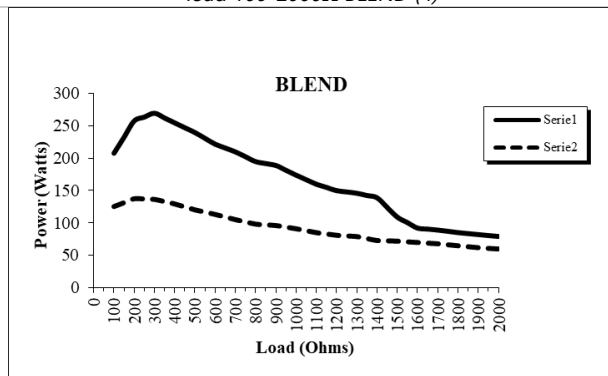
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (3)



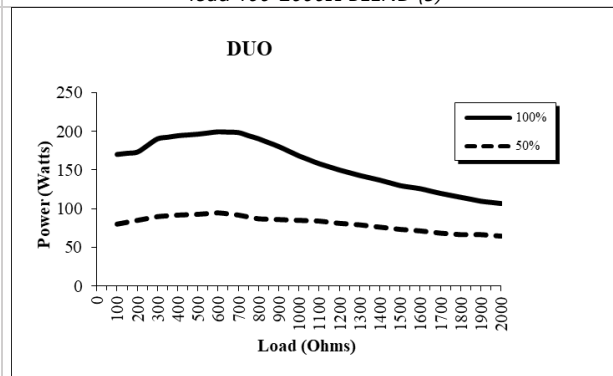
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (4)



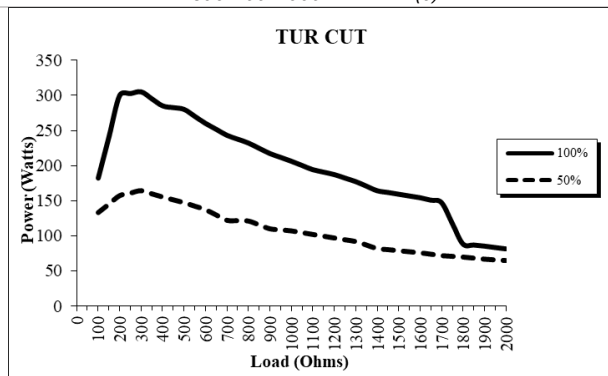
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (5)



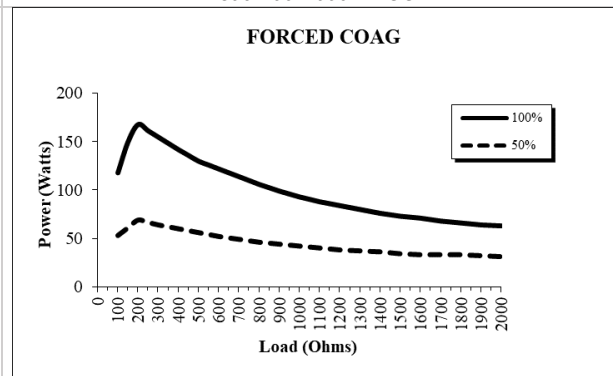
Diagrams of half and maximum output power versus impedance load 100-2000Ω BLEND (6)



Diagrams of half and maximum output power versus impedance load 100-2000Ω DUO

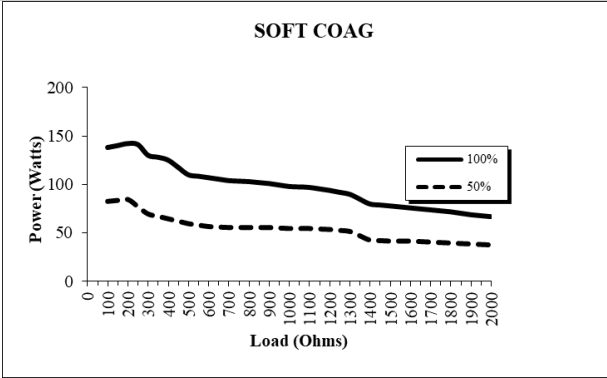


Diagrams of half and maximum output power versus impedance load 100-2000Ω TUR CUT

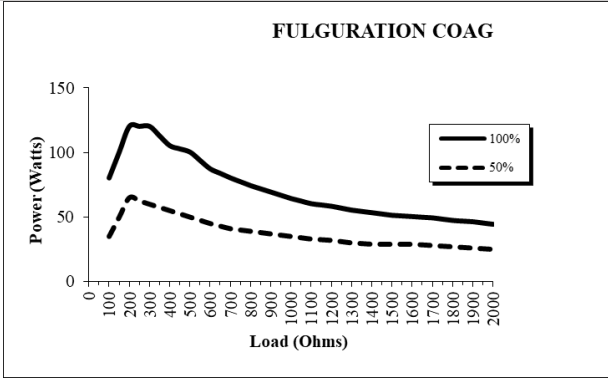


Diagrams of half and maximum output power versus impedance load 100-2000Ω FORCED COAG

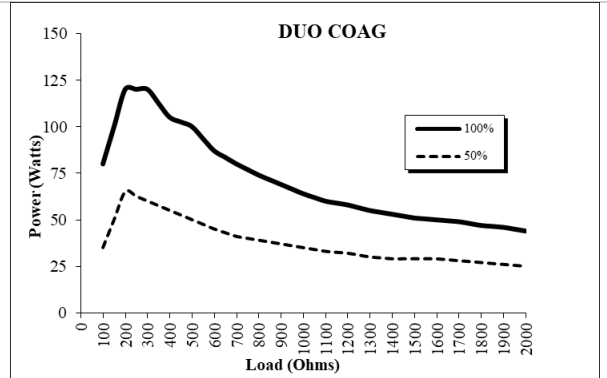
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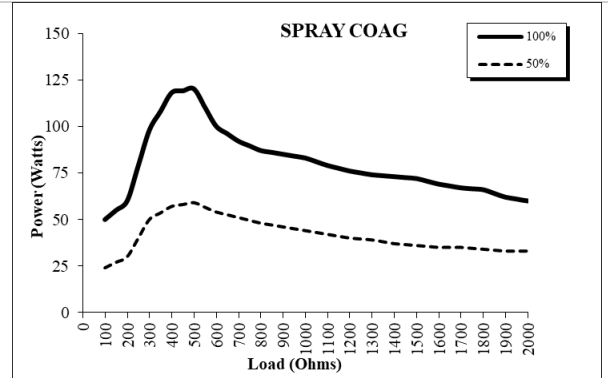
Diagrams of half and maximum output power versus impedance load 100-2000Ω SOFT COAG



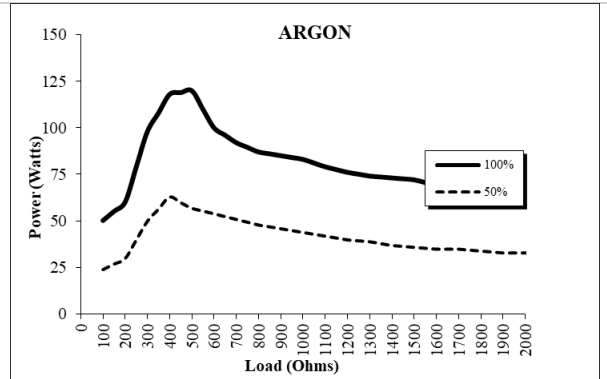
Diagrams of half and maximum output power versus impedance load 10-2000Ω FULGURATION



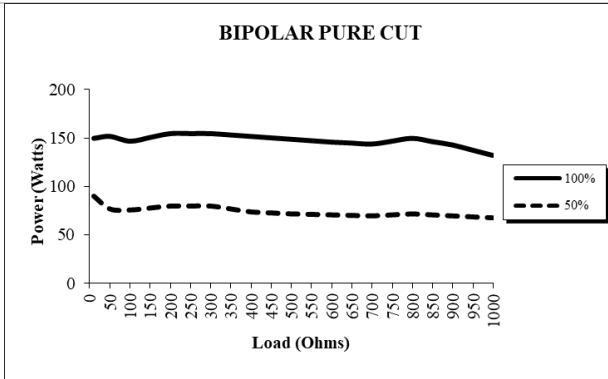
Diagrams of half and maximum output power versus impedance load 10-2000Ω DUO COAG



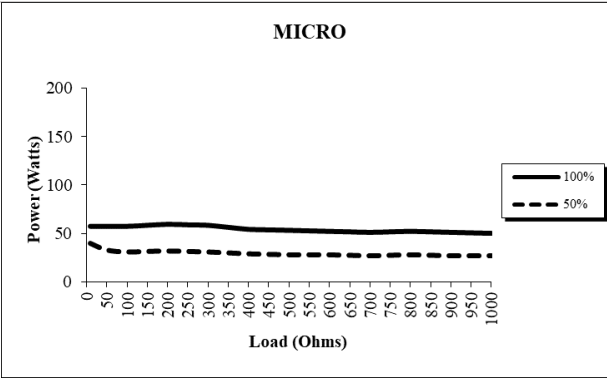
Diagrams of half and maximum output power versus impedance load 10-2000Ω SPRAY COAG



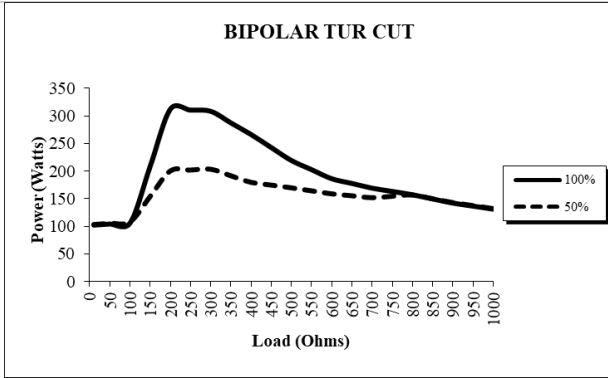
Diagrams of half and maximum output power versus impedance load 100-2000Ω ARGON



Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR CUT



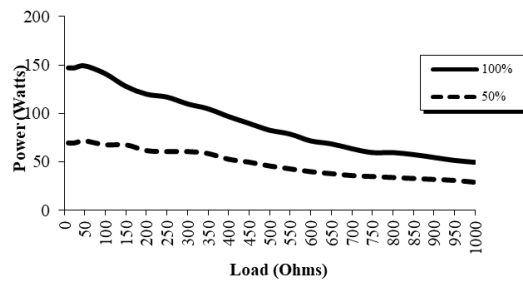
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR MICRO CUT



Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR TURCUT

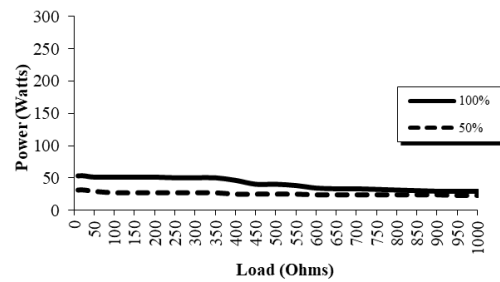
DIATERMO MB 400 T

BIPOLAR COAG



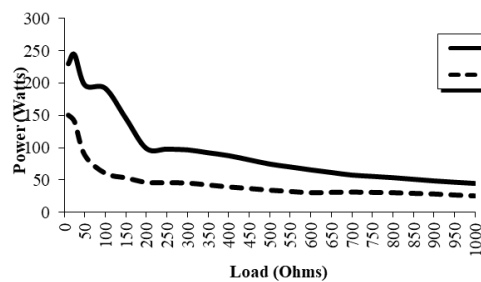
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR COAG

BIPOLAR MICRO COAG



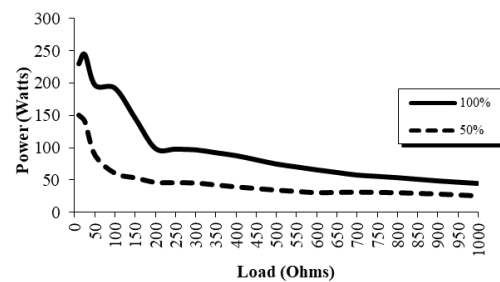
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR MICRO COAG

BIPOLAR TUR COAG



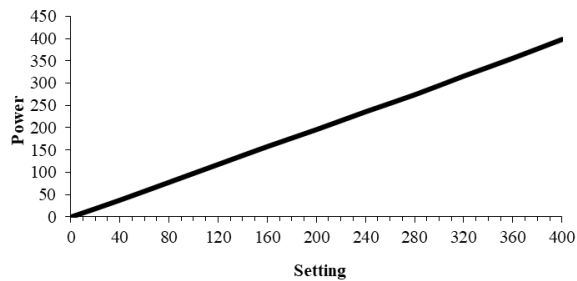
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR TUR COAG

BIPOLAR VESSEL COAG



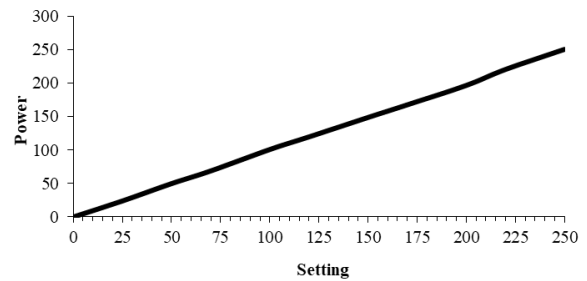
Diagrams of half and maximum output power versus impedance load 10-1000Ω BIPOLAR VESSEL

PURE CUT



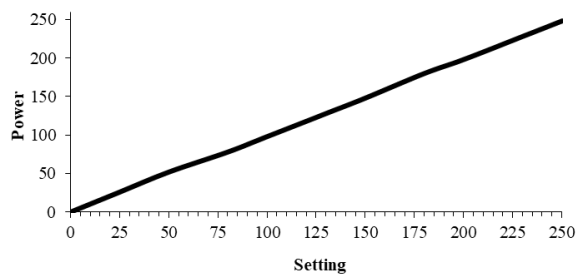
Diagrams of output power versus nominal value CUT100%

ENHANCED CUT



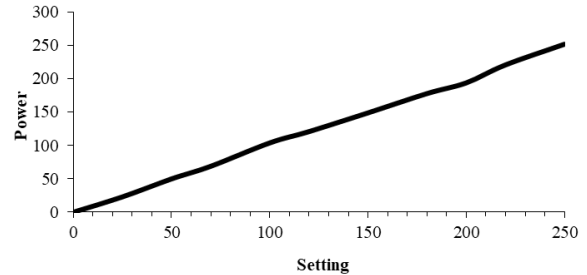
Diagrams of output power versus nominal value ENHANCED

BLEND CUT



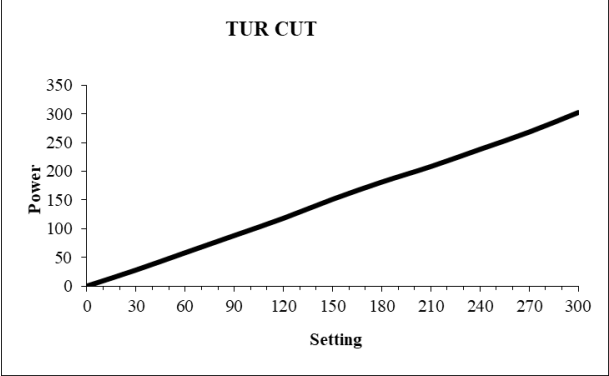
Diagrams of output power versus nominal value BLEND

DUO CUT

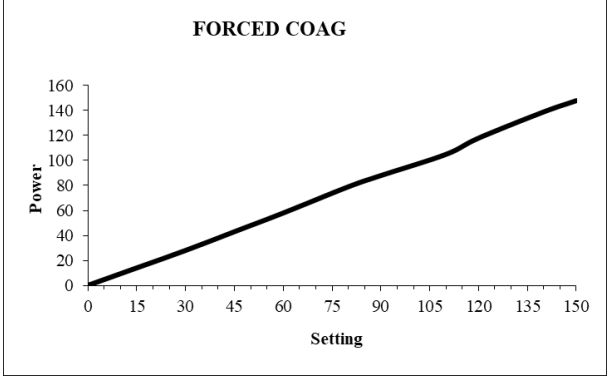


Diagrams of output power versus nominal value DUO CUT

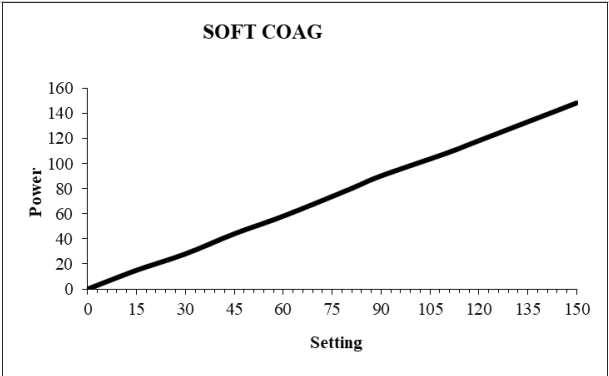
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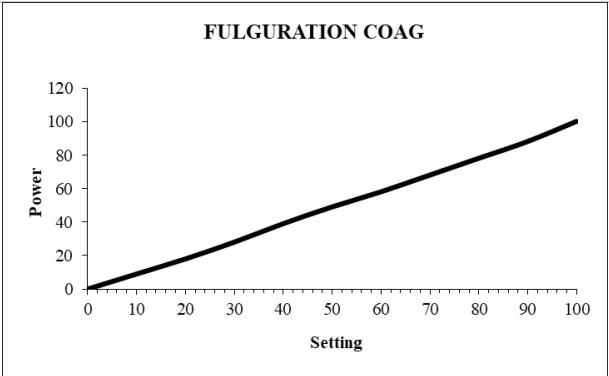
Diagrams of output power versus nominal value
TUR CUT



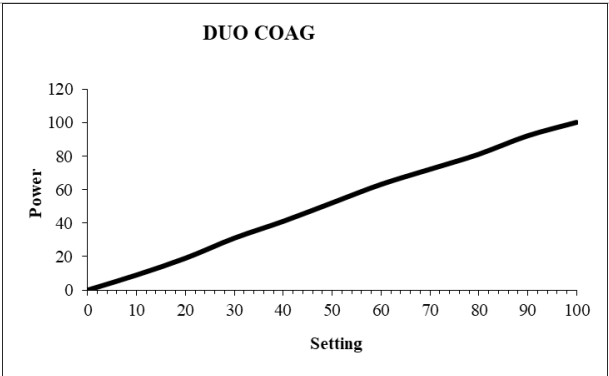
Diagrams of output power versus nominal value
FORCED COAG



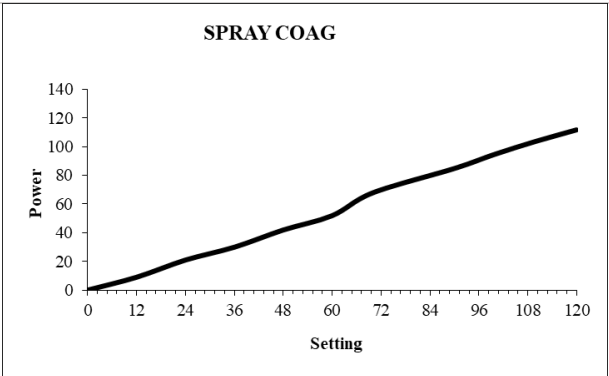
Diagrams of output power versus nominal value
SOFT COAG



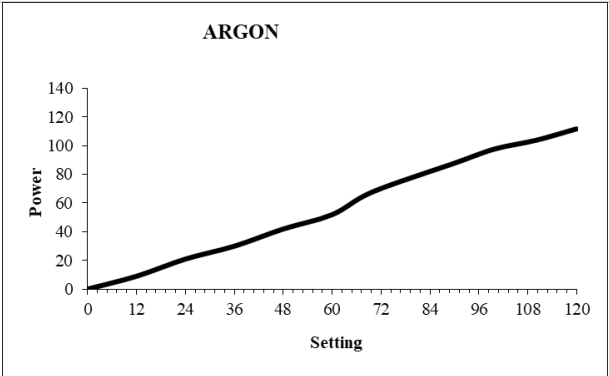
Diagrams of output power versus nominal value
FULGURATION



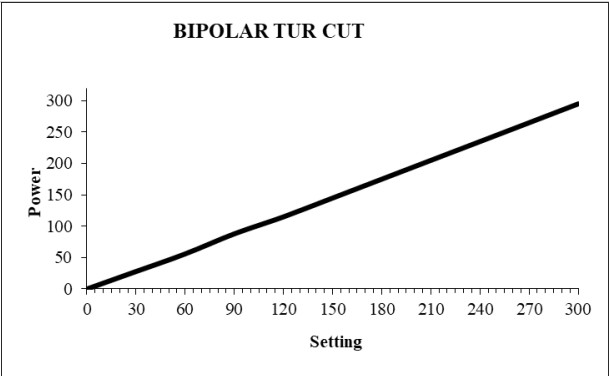
Diagrams of output power versus nominal value
DUO COAG



Diagrams of output power versus nominal value
SPRAY



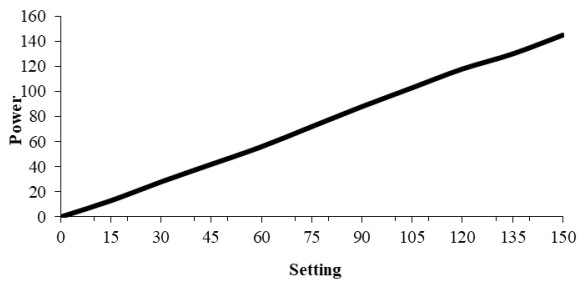
Diagrams of output power versus nominal value
ARGON



Diagrams of output power versus nominal value
BIPOLAR TURCUT

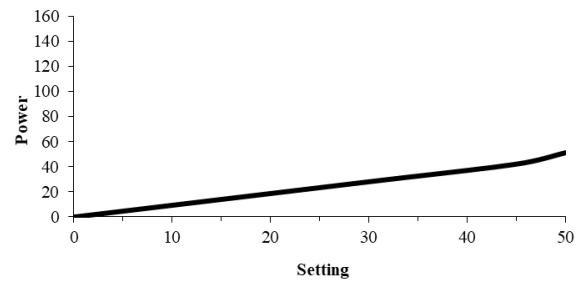
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BIPOLAR COAG



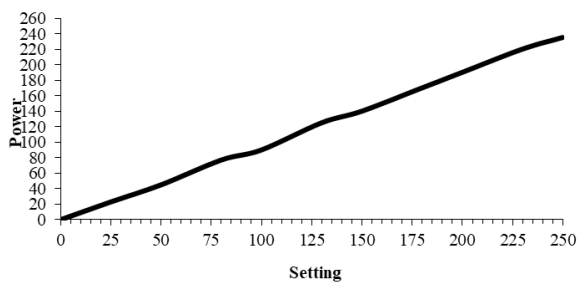
Diagrams of output power versus nominal value
BIPOLAR COAG

BIPOLAR MICRO CUT



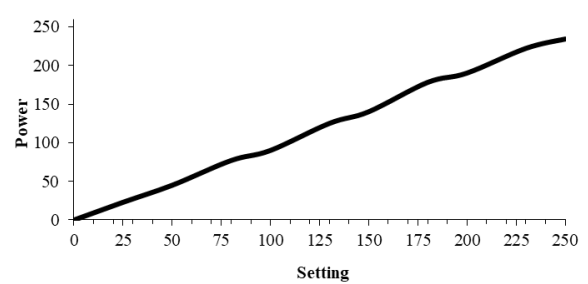
Diagrams of output power versus nominal value
BIPOLAR MICRO COAG

BIPOLAR TUR COAG



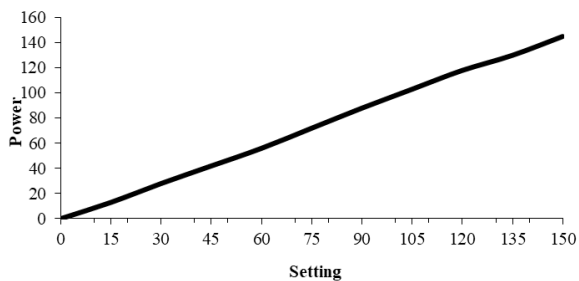
Diagrams of output power versus nominal value
BIPOLAR TUR COAG

BIPOLAR VESSEL SEALING



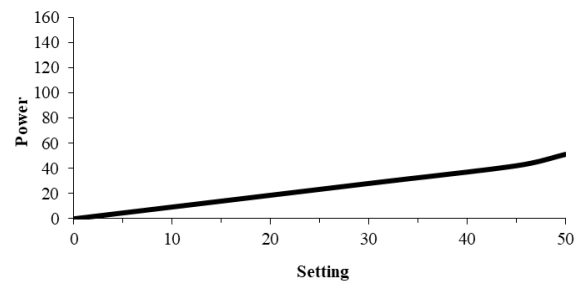
Diagrams of output power versus nominal value
BIPOLAR VESSEL

BIPOLAR COAG



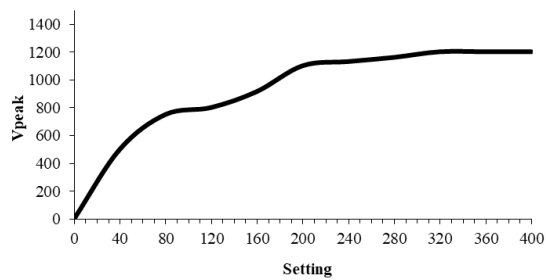
Diagrams of output power versus nominal value
BIPOLAR COAG

BIPOLAR MICRO CUT



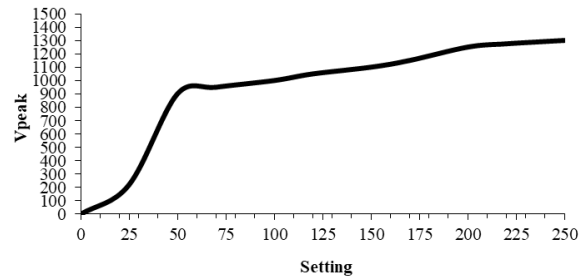
Diagrams of output power versus nominal value
BIPOLAR MICRO COAG

PURE CUT



Diagrams of maximum mains voltage output versus Vp
CUT 100%

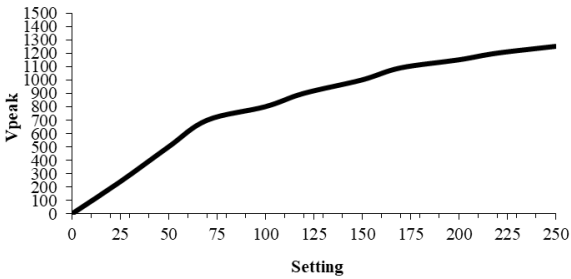
ENHANCED CUT



Diagrams of maximum mains voltage output versus Vp
ENHANCED

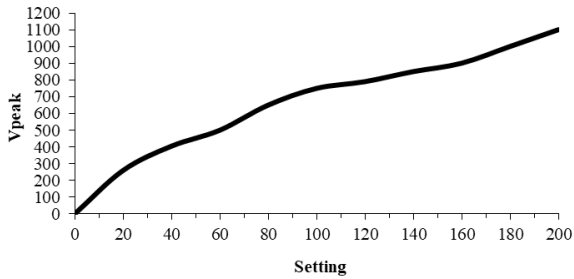
DIATERMO MB 400 T

BLEND CUT



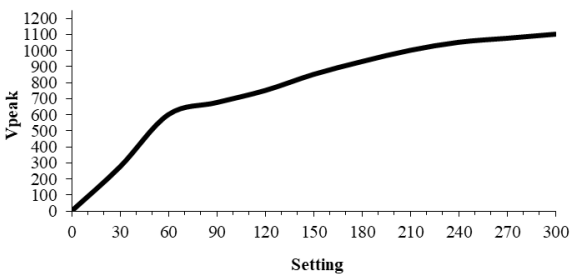
Diagrams of maximum mains voltage output versus Vp
BLEND

DUO CUT



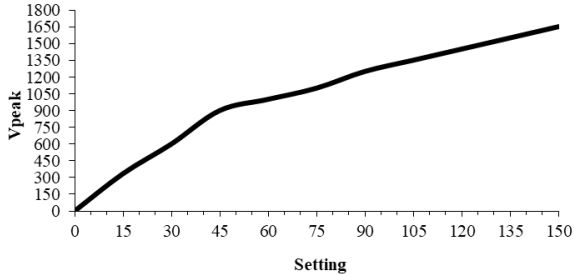
Diagrams of maximum mains voltage output versus Vp
DUO CUT

TUR CUT



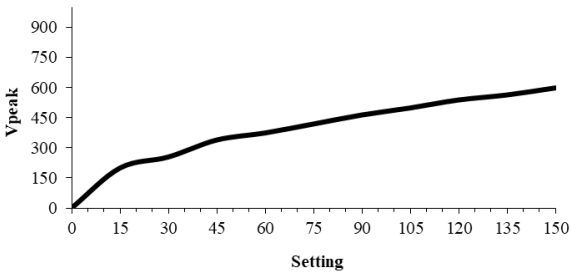
Diagrams of maximum mains voltage output versus Vp
TUR CUT

FORCED COAG



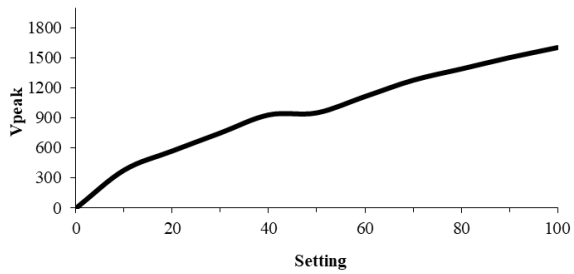
Diagrams of maximum mains voltage output versus Vp
FORCED COAG

SOFT COAG



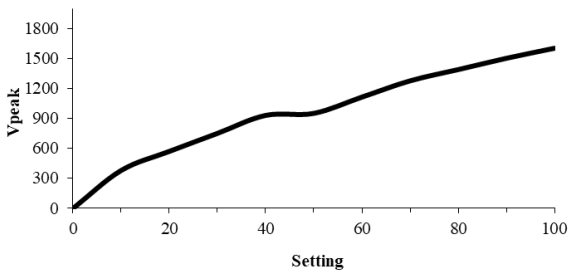
Diagrams of maximum mains voltage output versus Vp
SOFT COAG

FULGURATION COAG



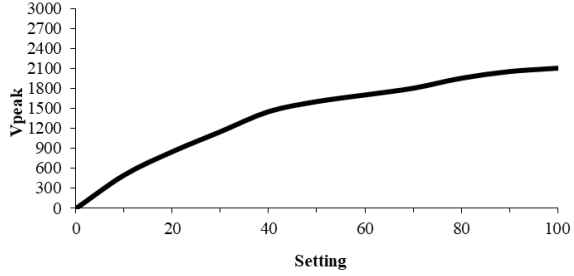
Diagrams of maximum mains voltage output versus Vp
FULGURATION

DUO COAG



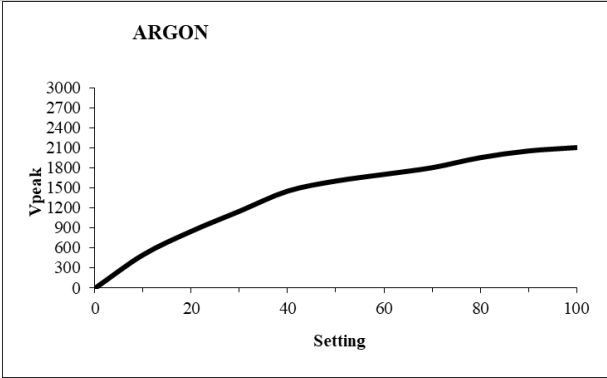
Diagrams of maximum mains voltage output versus Vp
DUO COAG

SPRAY COAG

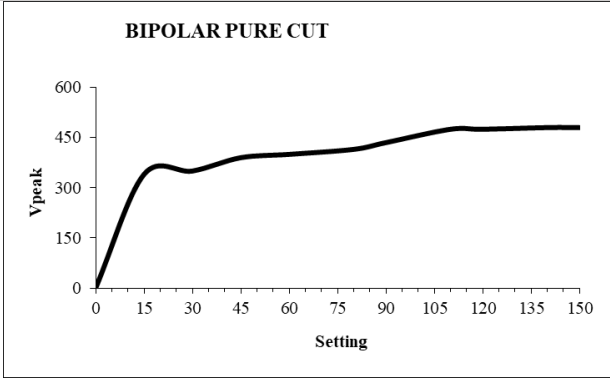


Diagrams of maximum mains voltage output versus Vp
SPRAY

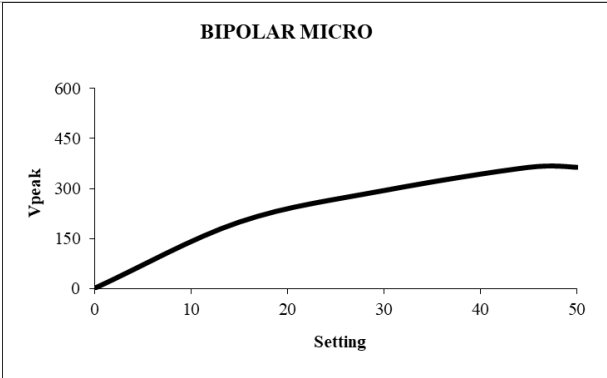
DIATERMO MB 400 T



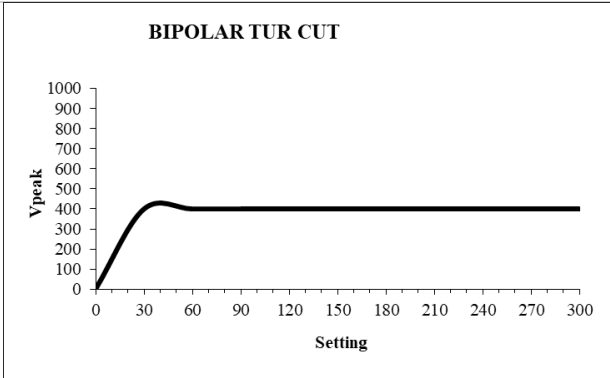
Diagrams of maximum mains voltage output versus Vp
ARGON



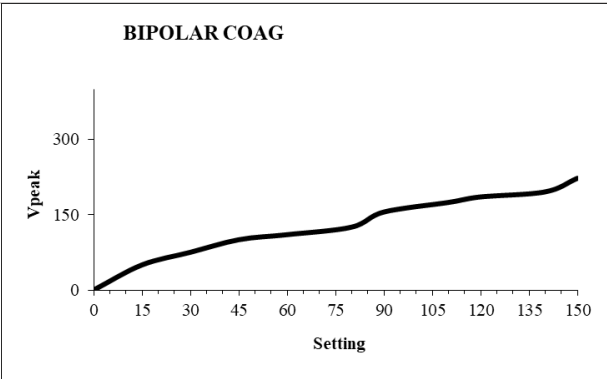
Diagrams of maximum mains voltage output versus Vp
BIPOLAR CUT



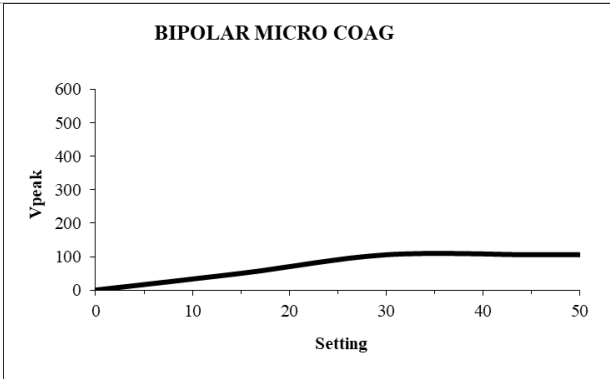
Diagrams of maximum mains voltage output versus Vp
BIPOLAR MICRO CUT



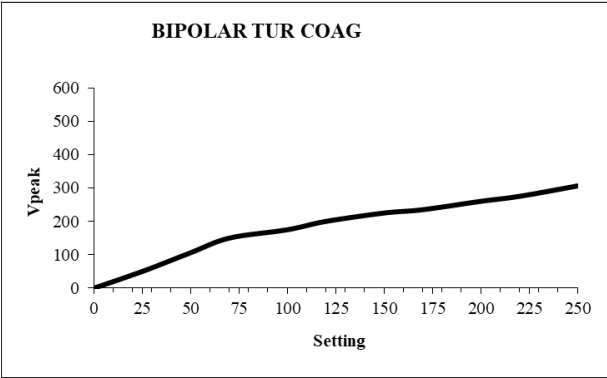
Diagrams of maximum mains voltage output versus Vp
BIPOLAR TUR



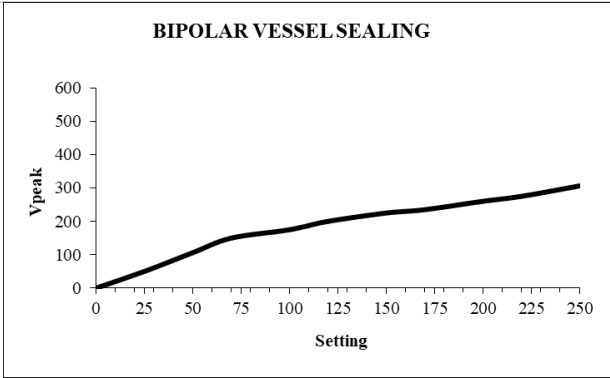
Diagrams of maximum mains voltage output versus Vp
BIPOLAR COAG



Diagrams of maximum mains voltage output versus Vp
BIPOLAR MICRO COAG



Diagrams of maximum mains voltage output versus Vp
BIPOLAR TUR COAG



Diagrams of maximum mains voltage output versus Vp
BIPOLAR VESSEL

**Information about elimination of this product
(Applicable in the countries with separate collection systems)**



On the end of the life, the present product mustn't be eliminated as urban refusal, but it must be eliminated in a separated collection.

If the product is eliminated in unsuitable way, it is possible that some parts of the product (for example some accumulators) could be negative for the environment and for the human health.

The symbol on the side (barred dustbin on wheel) denotes that the products mustn't throw into urban refuses container, but it must be eliminated with separate collection.

In case of abusive elimination of this product, could be foreseen sanctions.

Official Dealer

GIMA SPA

via Marconi, 1
20060 Gessate (MI) - Italy
gima@gimaitaly.com – export@gimaitaly.com
Phone +39 02 9538541
Fax +39 02 95381167
www.gimaitaly.com

